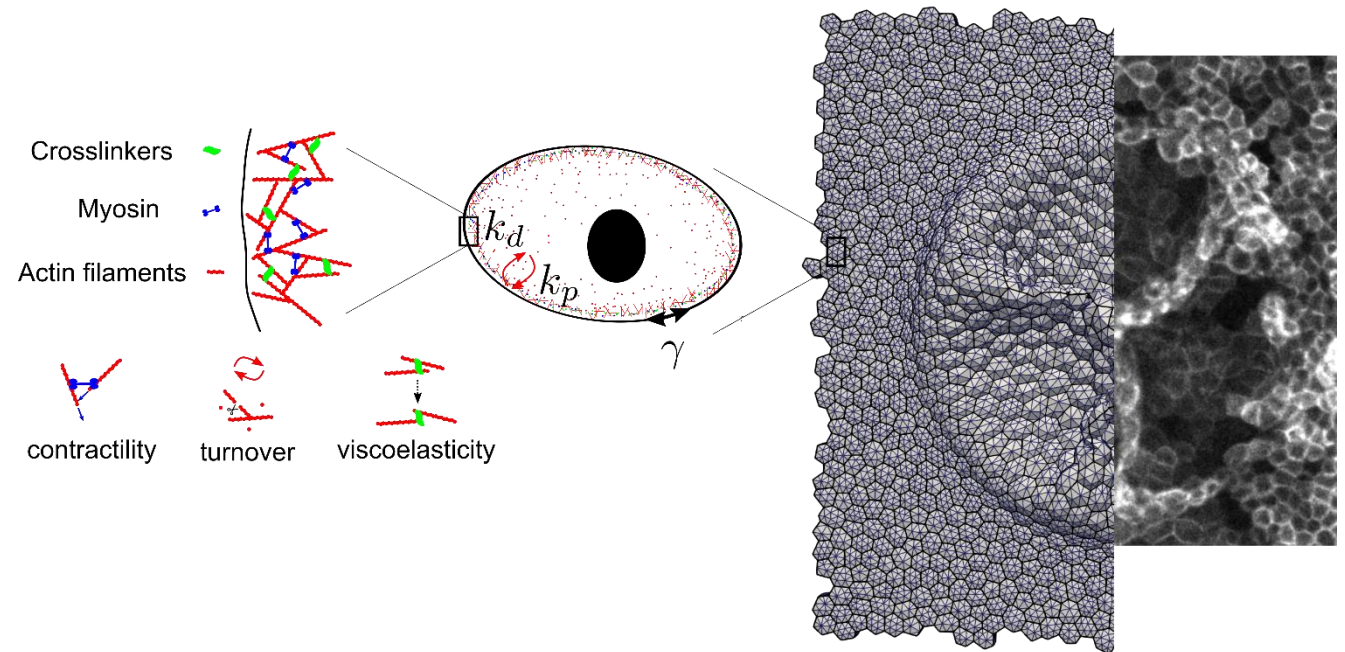


Wrinkling of epithelial shells: experiments, models, simulations

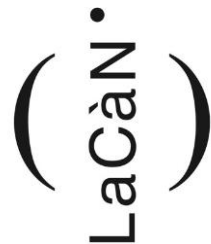
Adam Ouzeri

Rencontre GDR -GDM – Novembre 2025

Collaborators : Sohan Kale, Alejandro Torres-Sanchez, Daniel Santos-Oliván, Pradeep Bal, Guillermo Vilanova, Marino Arroyo, Nimesh Chahare, Xavier Trepas



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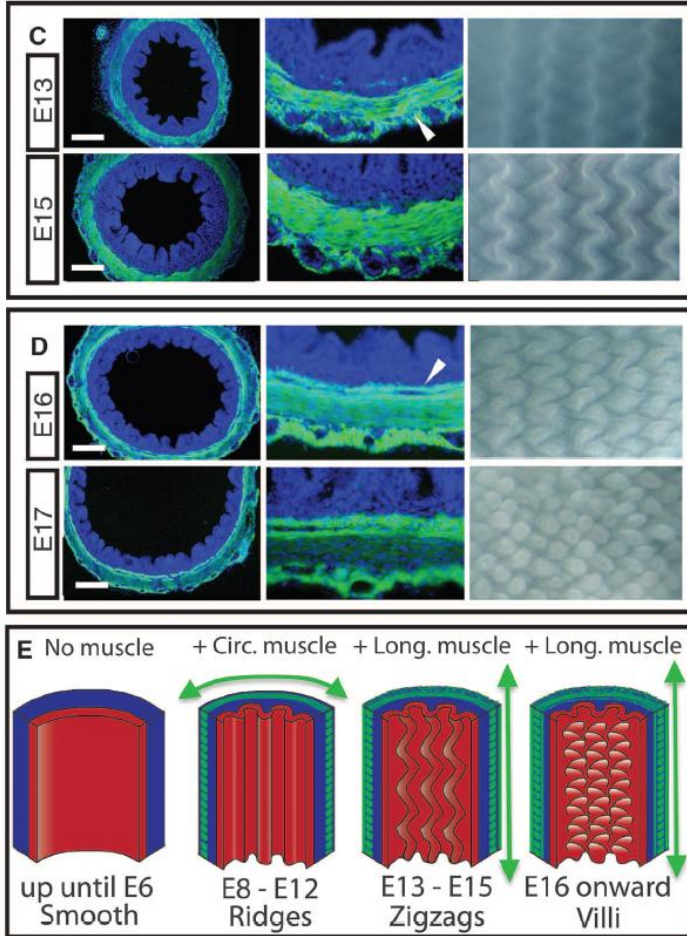
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UNIVERSITÉ



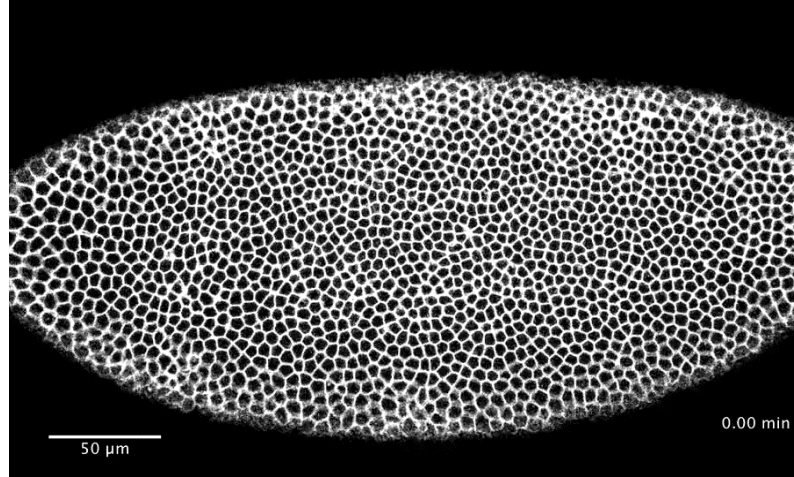
Outline

- Biological context
- *In vitro* experiments
- Vertex model
- Continuum approximation

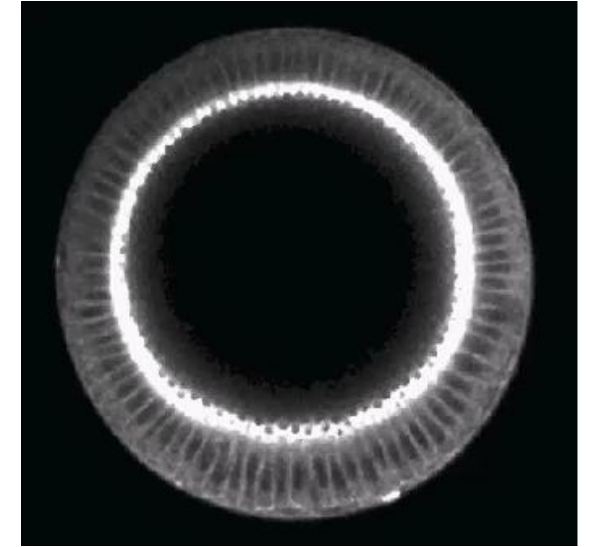
Mechanical instabilities as a driver of epithelial morphogenesis



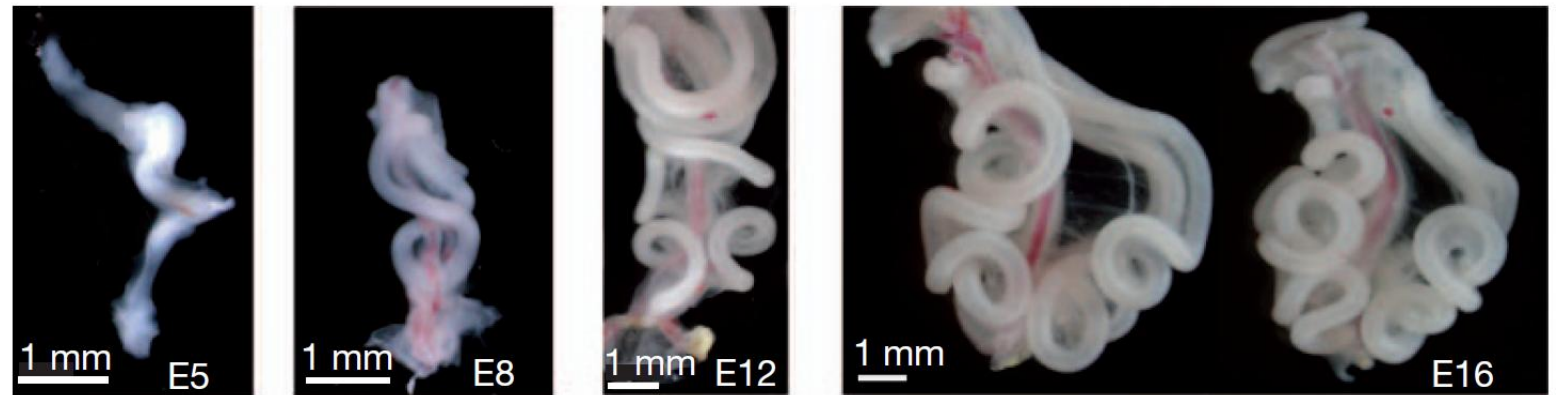
Shyer et al., Nature, 2011



Kazsa lab



Brodland et al., PNAS, 2010



Savin et al., Nature, 2011

-> fit as much surface area as possible in a confined space

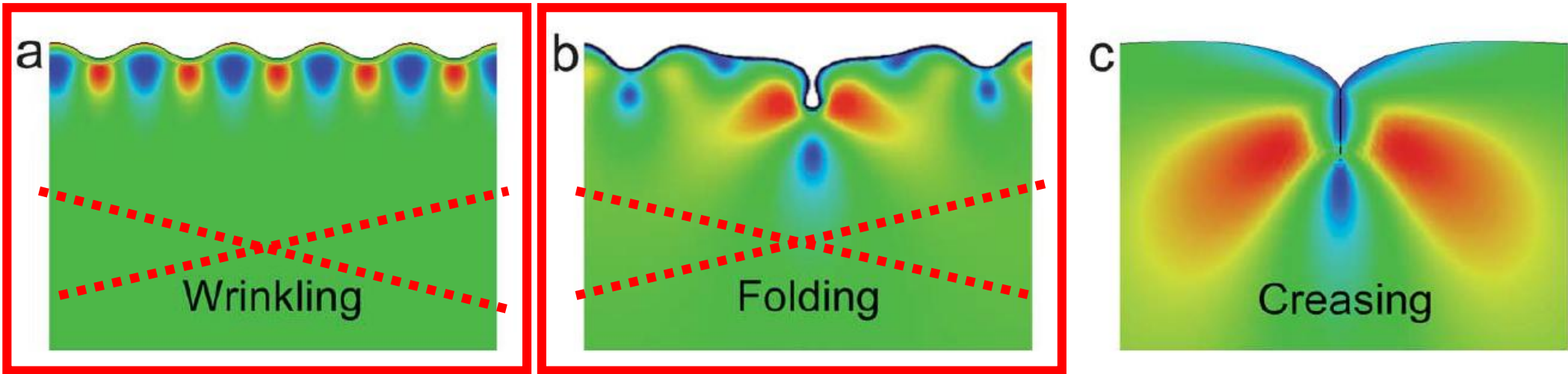
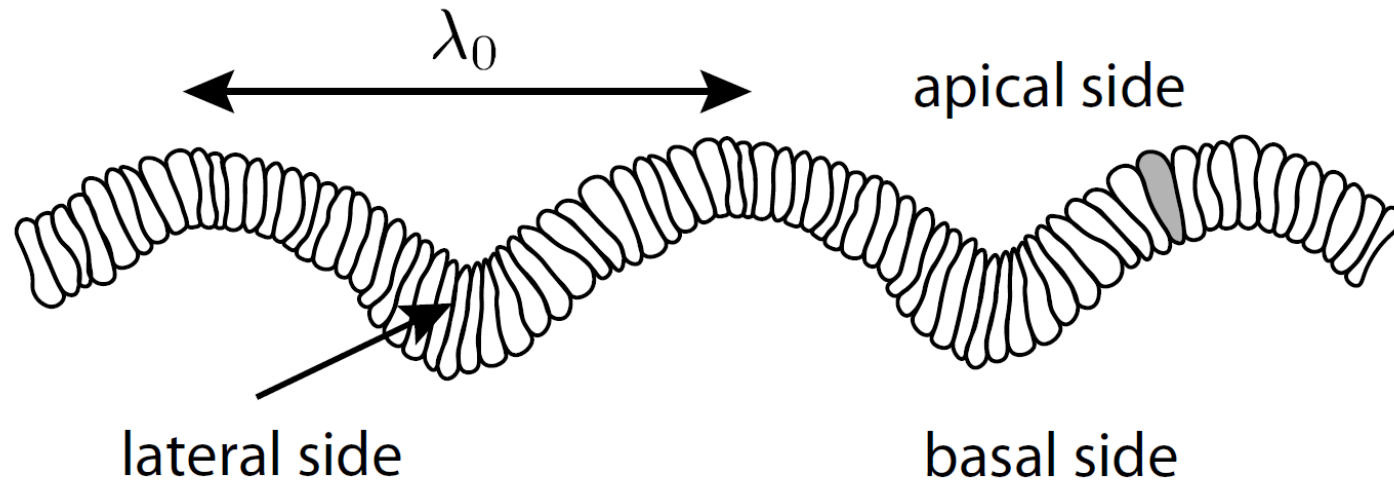


Fig. 1 Schematic of three types of morphological instability: (a) wrinkling, (b) folding, and (c) creasing.

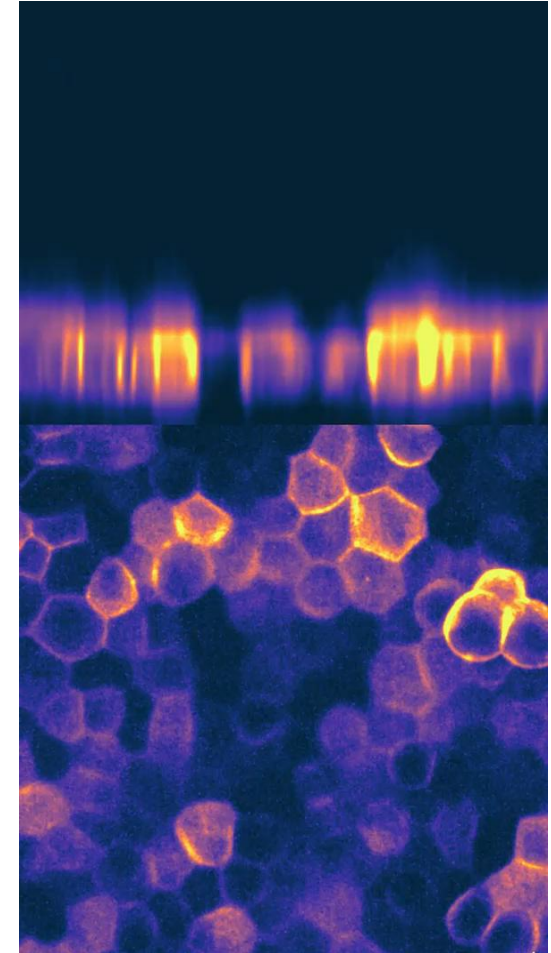
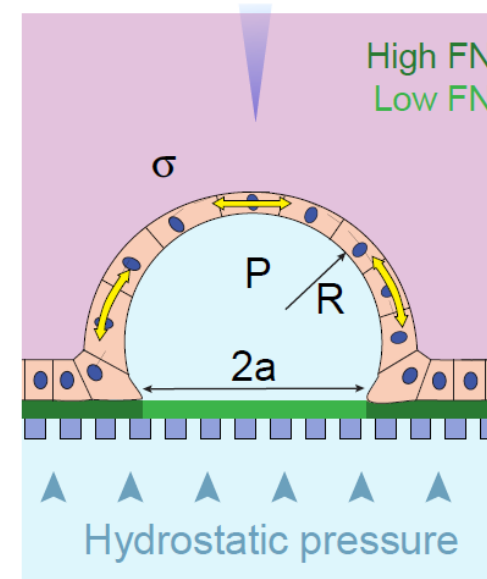
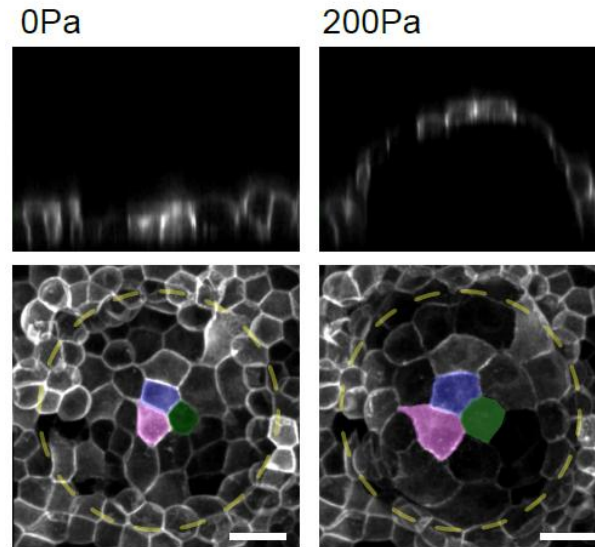
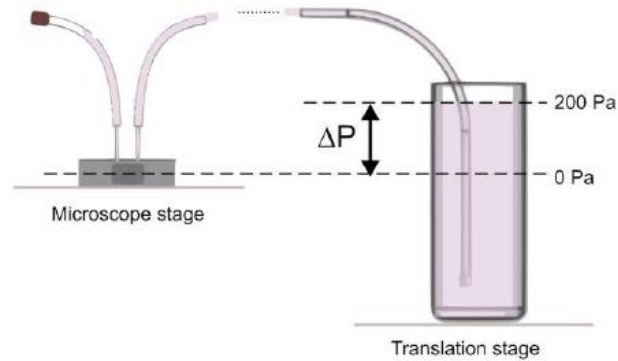
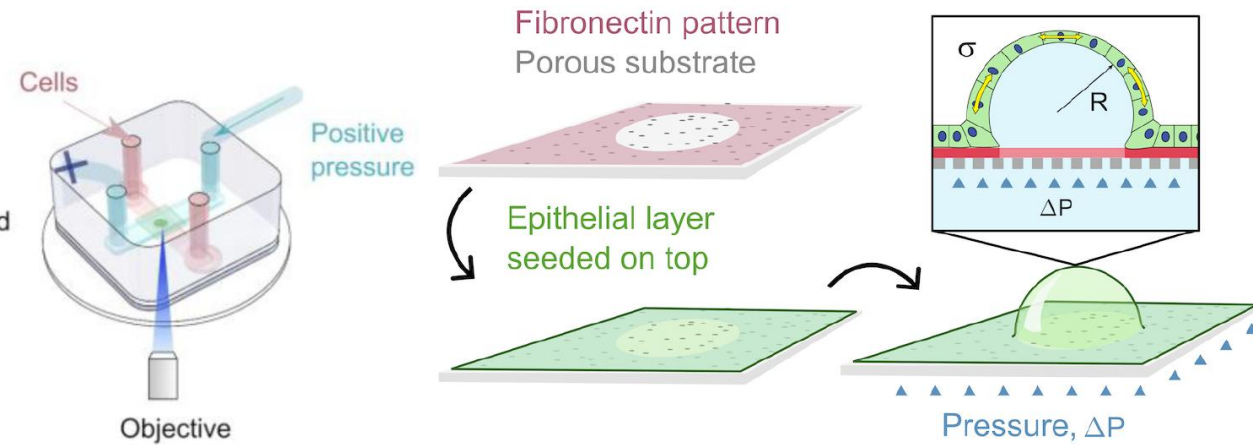
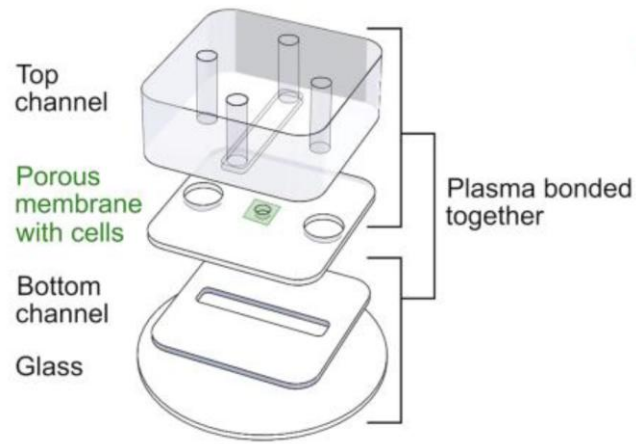
Li et al., Soft Matter, 2012



Wrinkling of unsupported monolayer in viscous medium

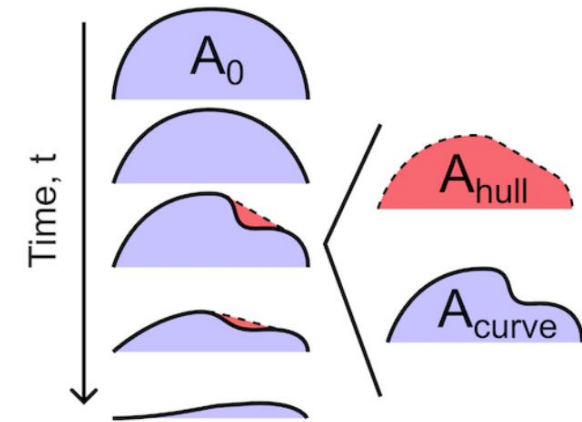
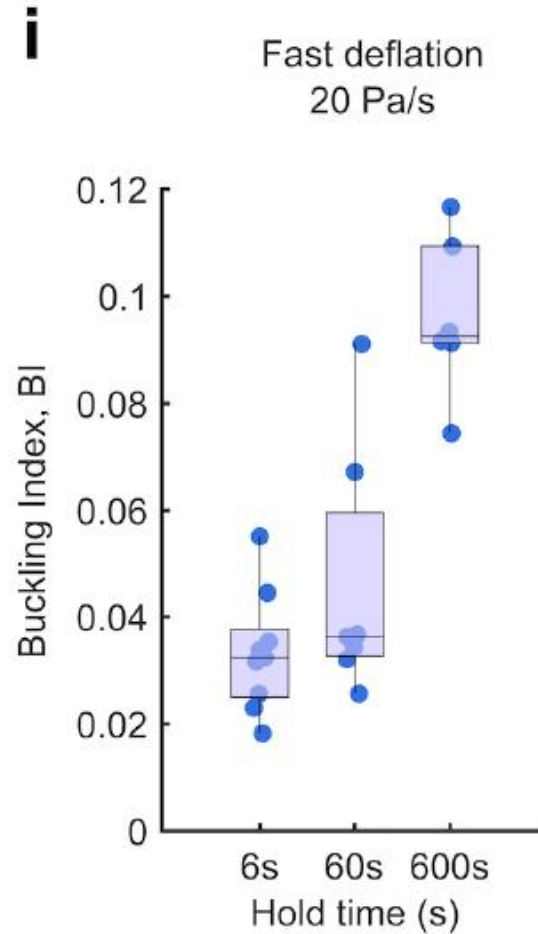
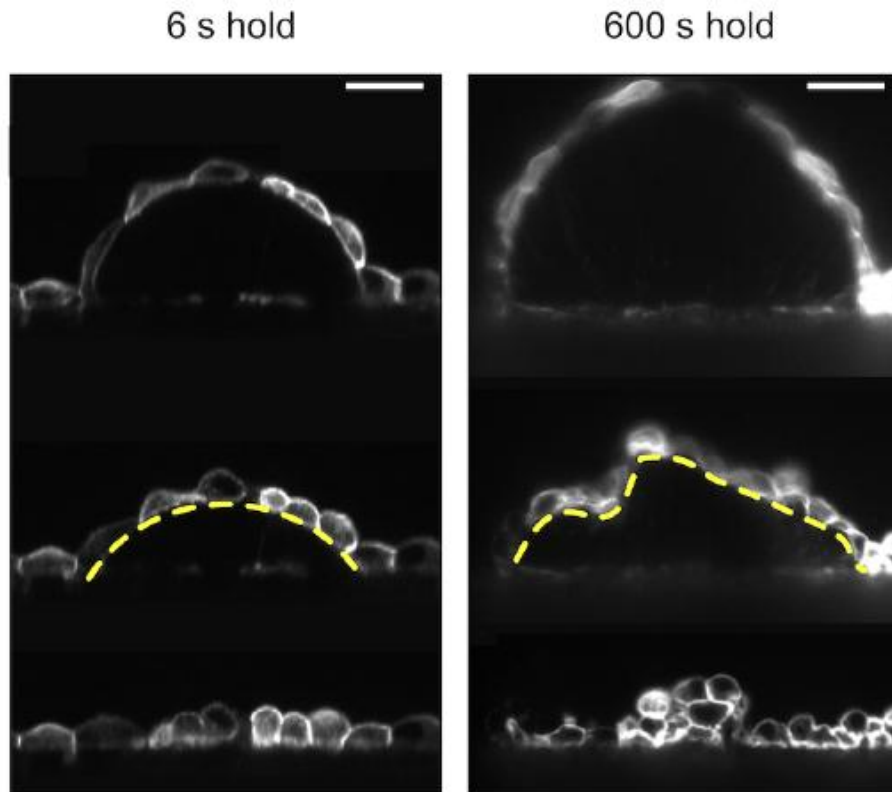
Andresek et al., PRL, 2023

Dynamical control of suspended monolayers



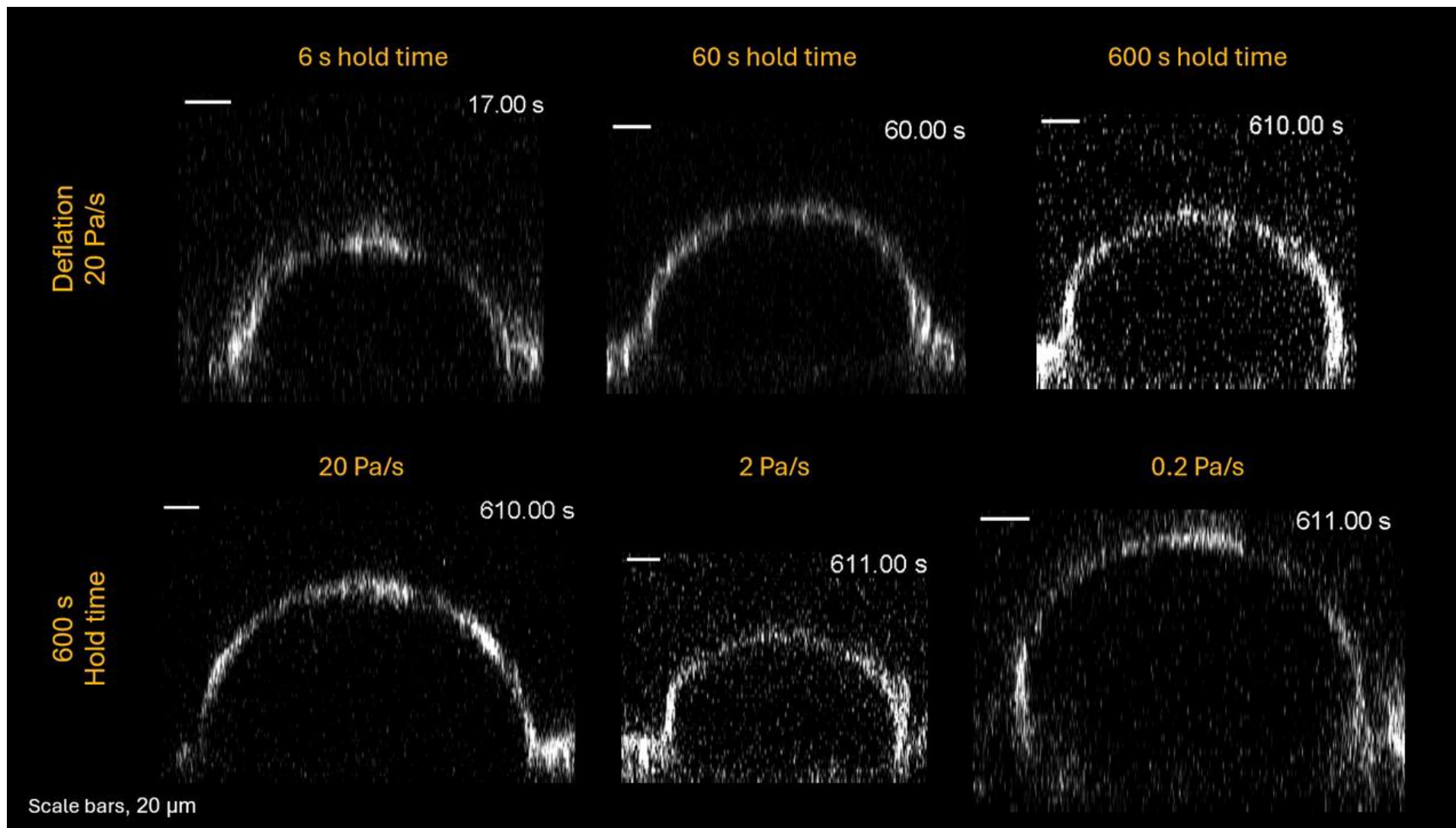
MOLI : Monolayer Inflator

Buckling depends on hold time

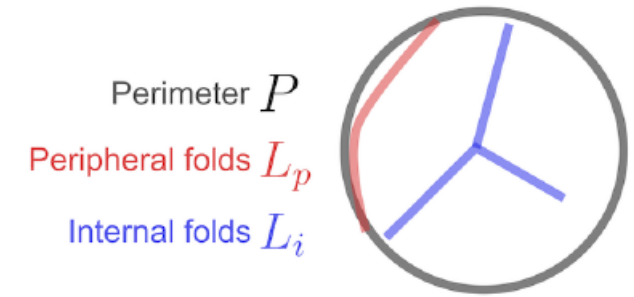
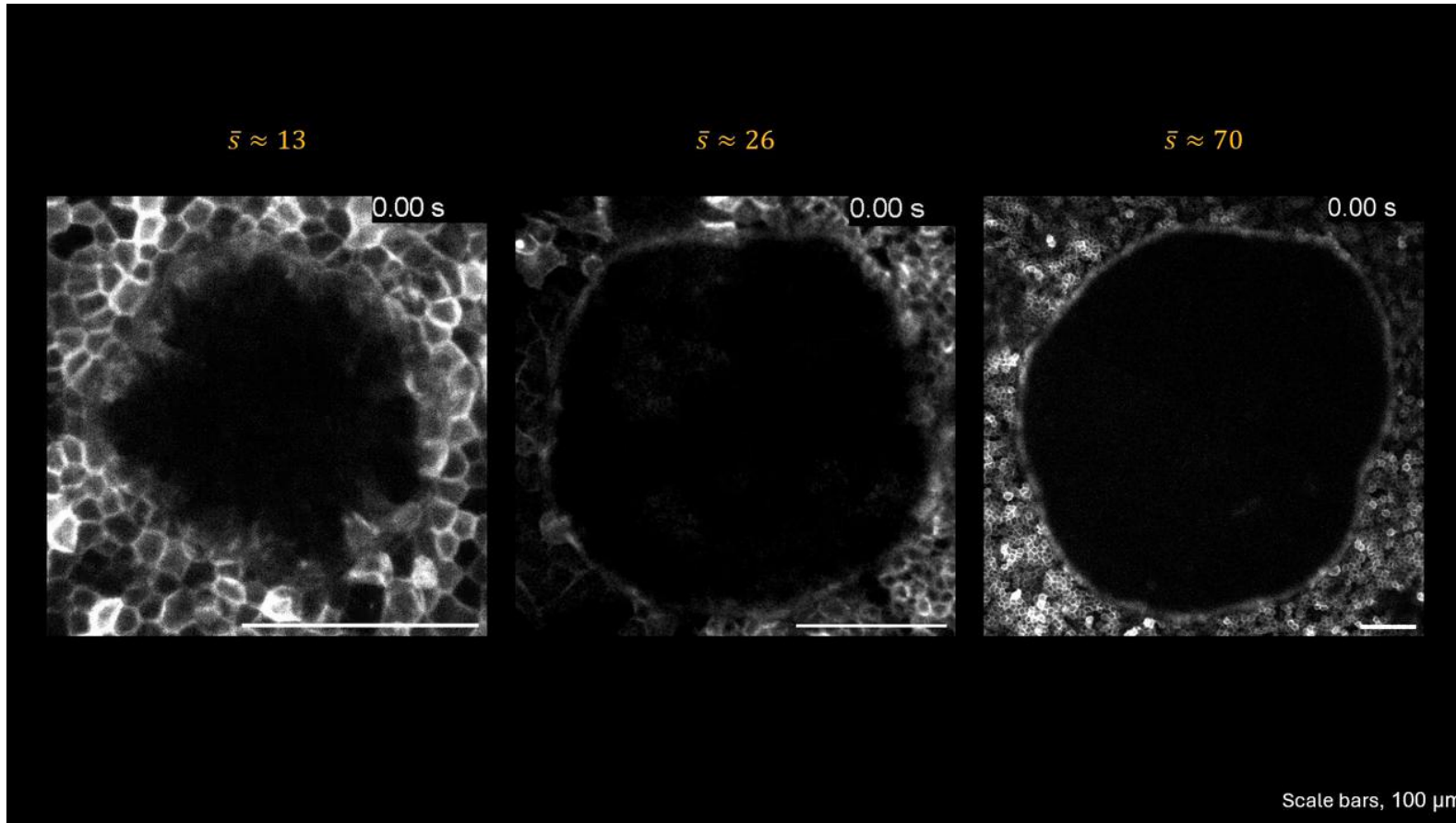
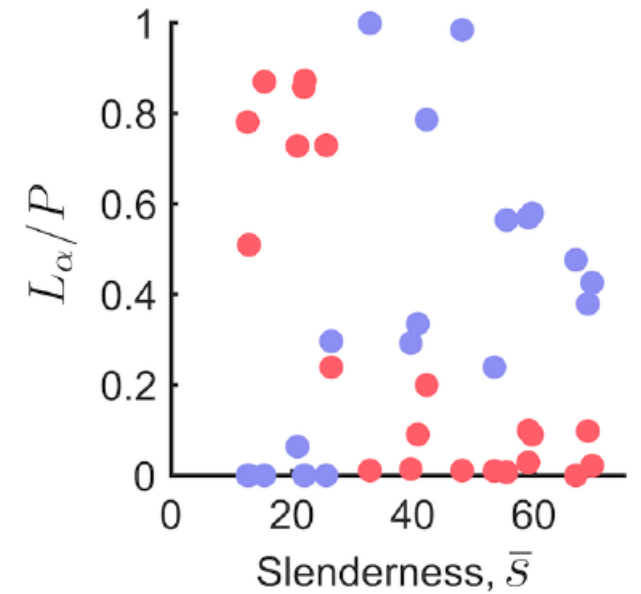


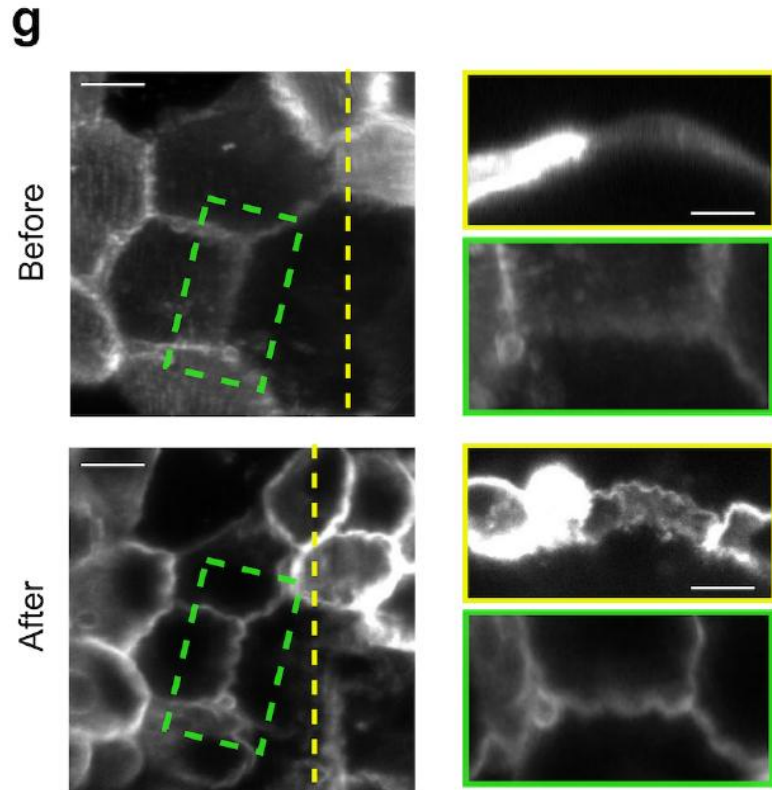
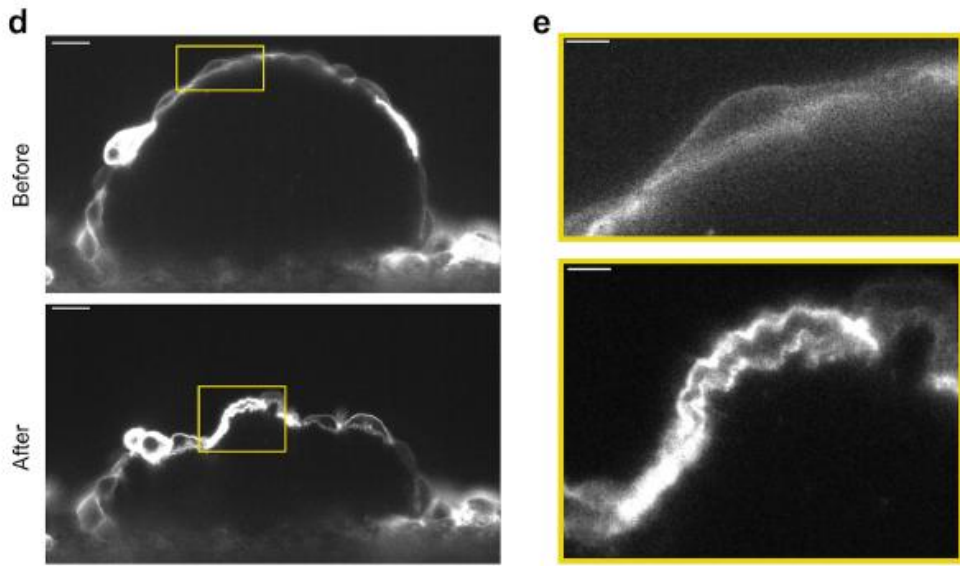
$$BI = \max_t \left\{ \frac{A_{\text{hull}}^t - A_{\text{curve}}^t}{A_0} \right\}$$

Buckling depends on deflation rate and hold time

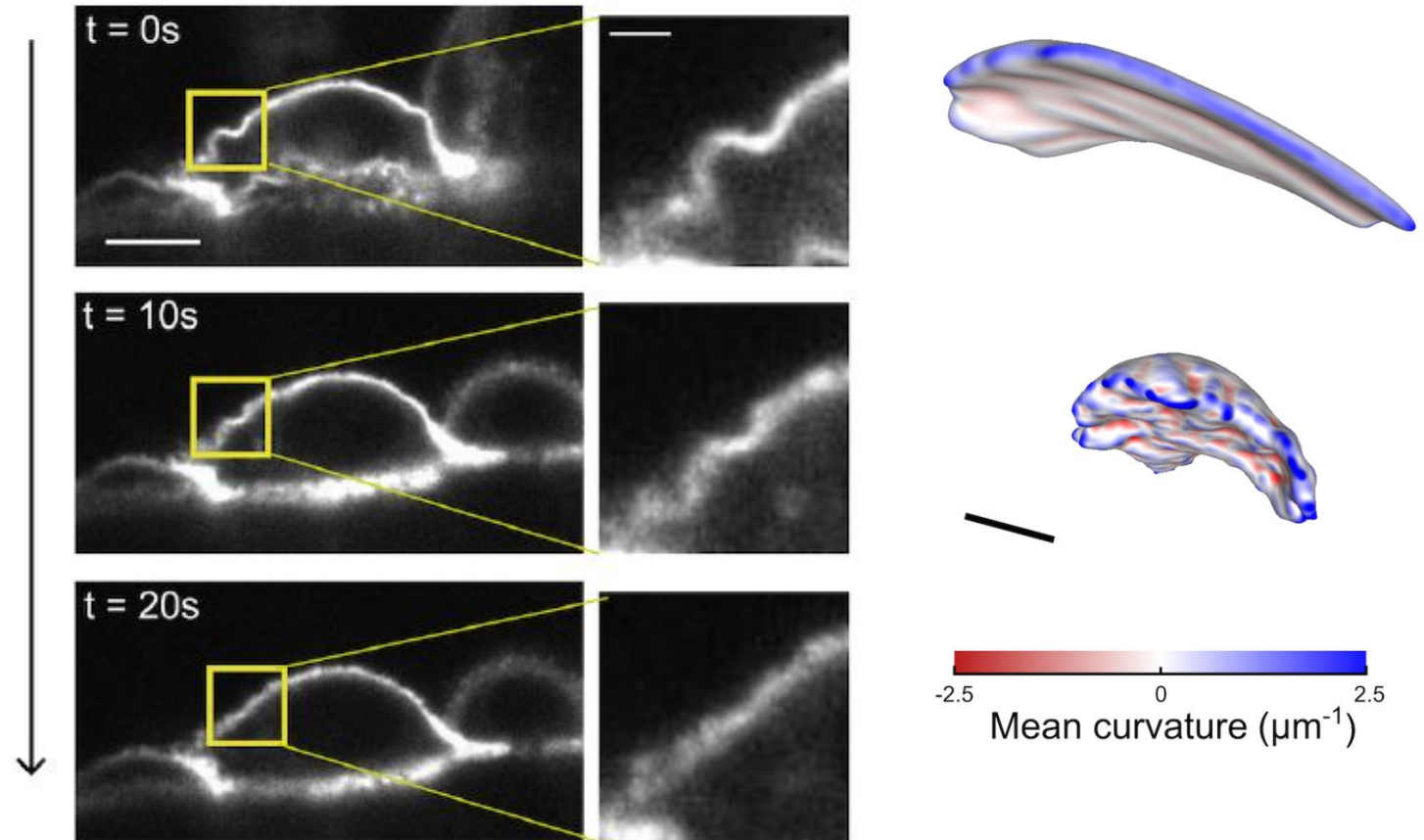


Symmetry-breaking and wrinkling pattern

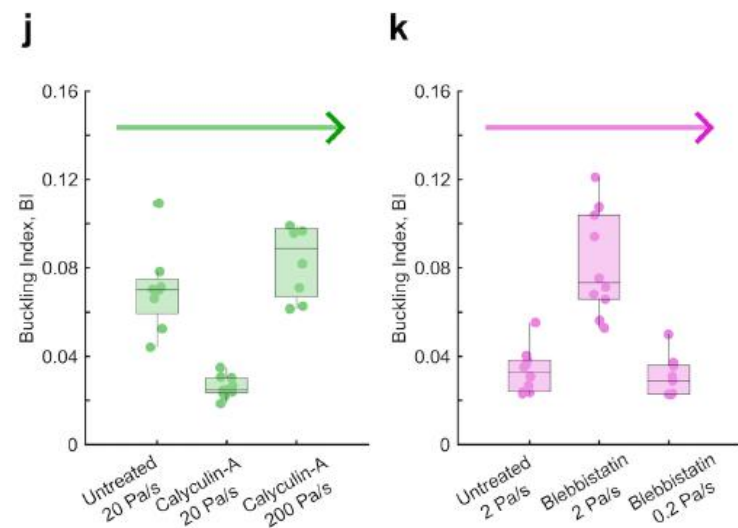
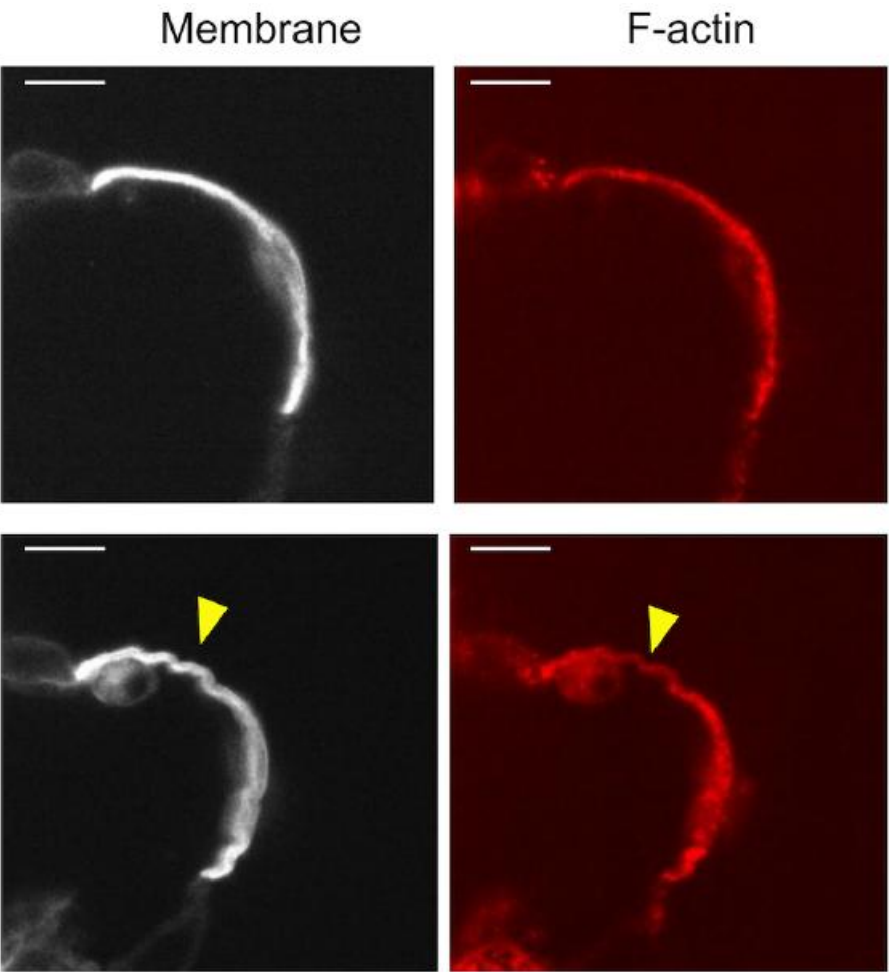
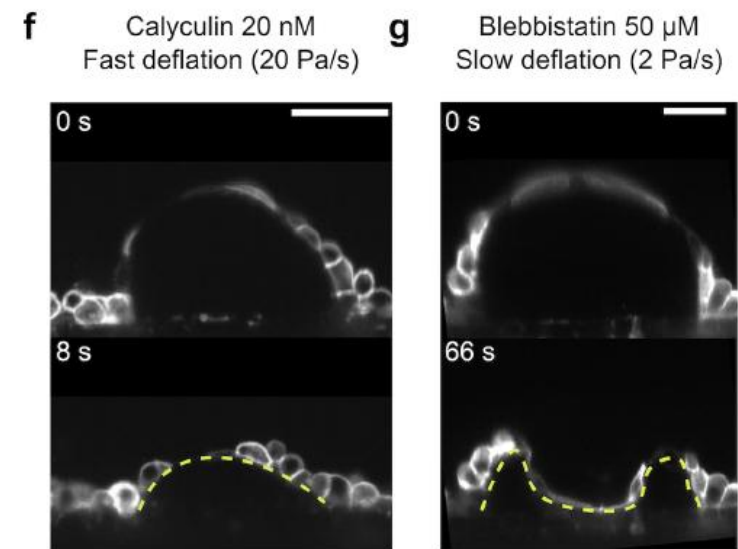
 L_α/P , where $\alpha = p, i$ 



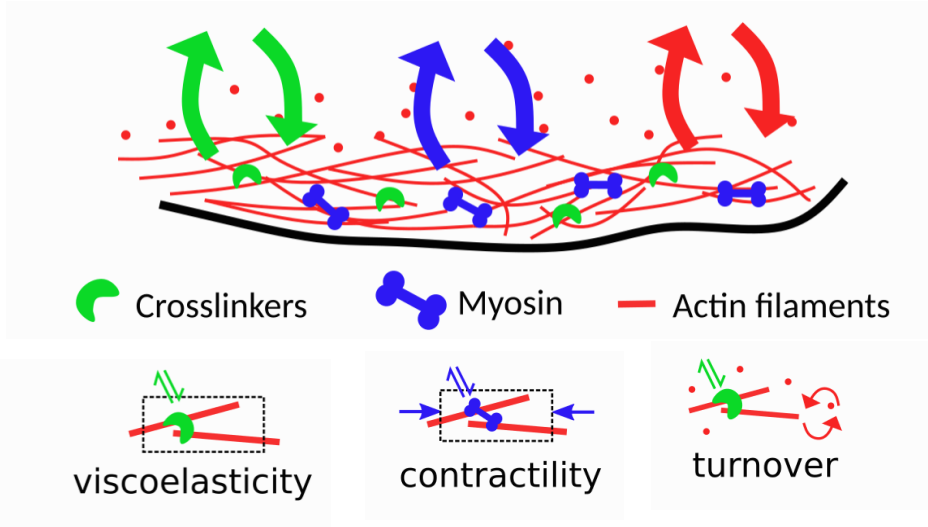
Wrinkling at multiple scales



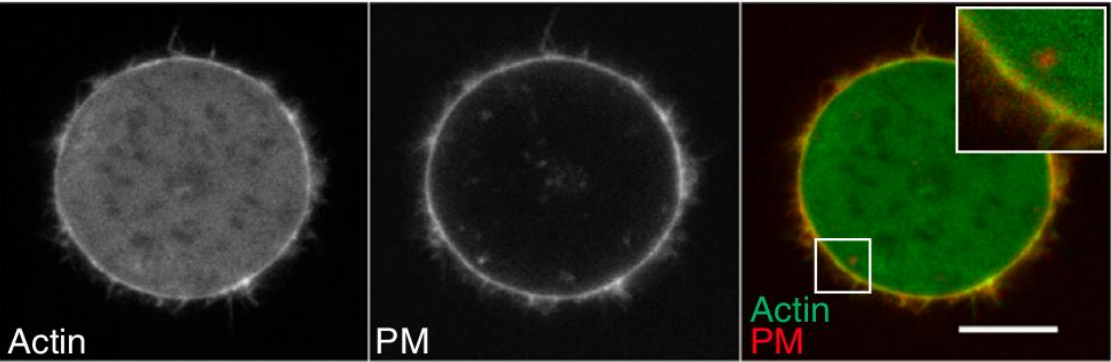
Buckling depends on the actomyosin cortex dynamics



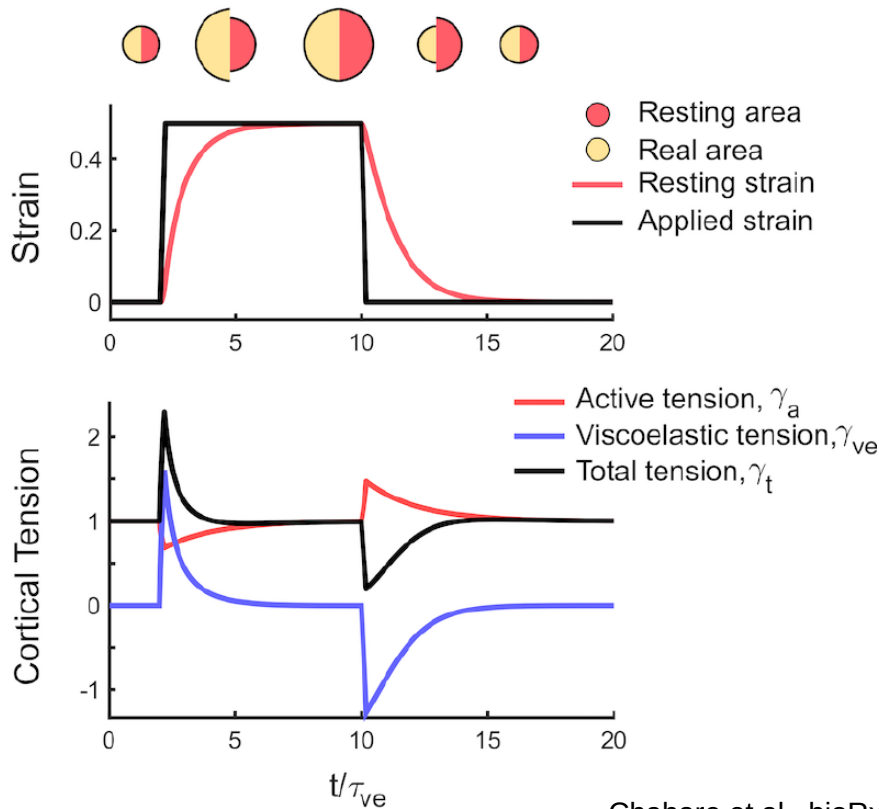
Actomyosin cortex



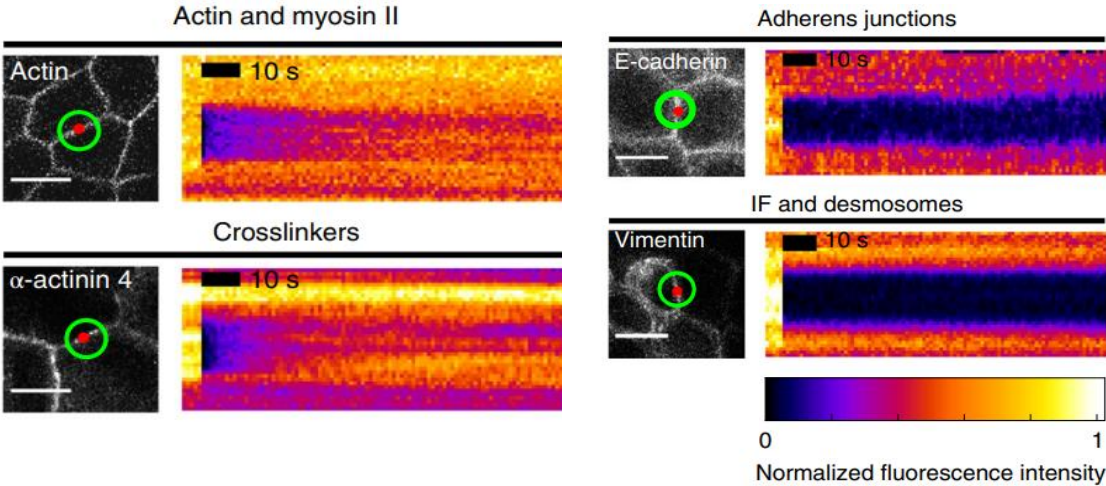
Ouzeri et al., bioRxiv., 2025



Clark, Dierkes, Paluch, Biophys. J., 2013

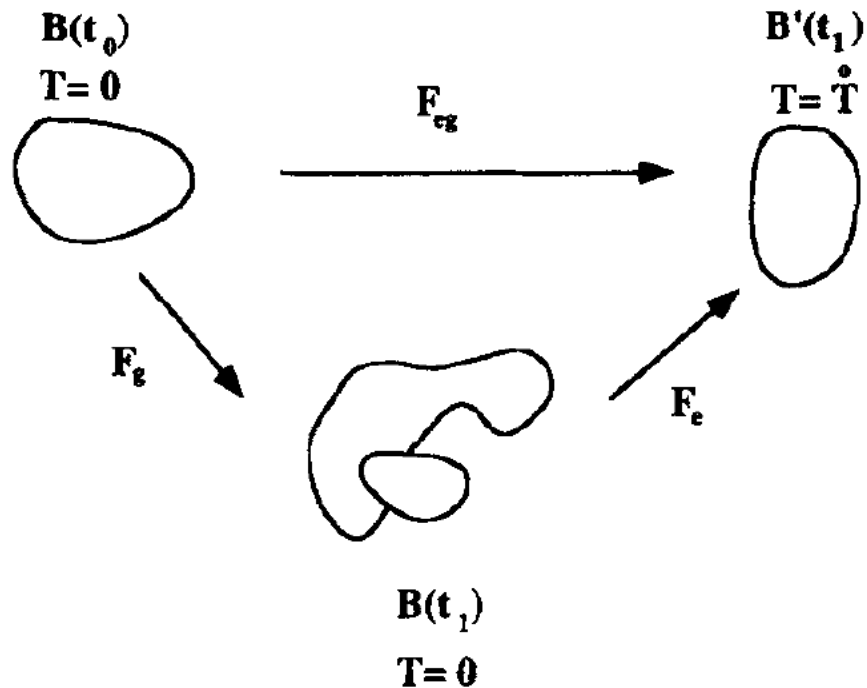


Chahare et al., bioRxiv., 2025

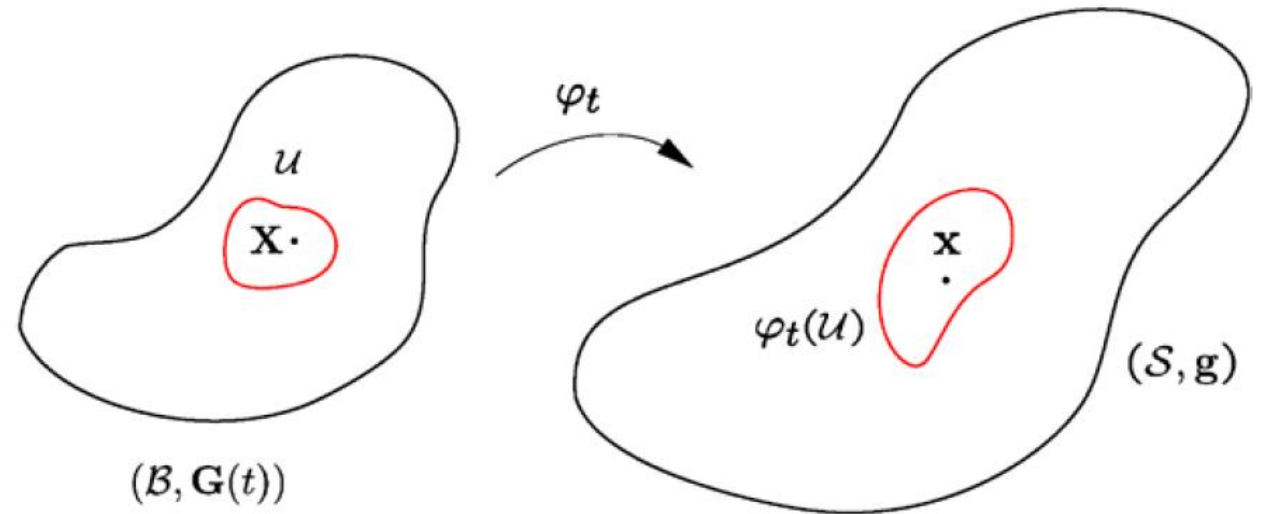


Khalilgharibi et al. Nat. Phys., 2019

Geometric approach to elastic growth (morphoelasticity)



Rodriguez et al., J. Biomechanics, 1994



-> Riemannian manifold whose metric is related to the growth and with respect to which strains should be measured

-> Time-dependent stress-free configuration

-> Evolution law ?

Onsager's variational principle

- Coupling multiple physics at multiple scales
- Applicable to a wide variety of biological settings
- Thermodynamically consistent models by construction

State and process variables

$$X, V \quad \partial_t X = V \text{ or } \partial_t X = P(X)V$$

Rate of change of free energy

$$\frac{dF(X(t))}{dt} = D_X \mathcal{F}(X) P(X)V$$

Dissipation potential $\mathcal{D}(X; V)$

Power input $\mathcal{P}(X; V) = -F(X)V$

$$\mathcal{L}(X; V, \Lambda) = \mathcal{R}(X; V) + \Lambda \cdot \mathbb{C}(X)V$$

$$\{V, \Lambda\} = \underset{W}{\operatorname{argmax}} \underset{\omega}{\operatorname{argmin}} [\mathcal{L}(X; W, \omega)]$$

1st and 2nd order (necessary) optimality conditions

$$\partial_V \mathcal{R} = 0 \quad \partial_V^2 \mathcal{R} = \partial_V^2 \mathcal{D} \geq 0$$

governing equations

2nd law of thermodynamics¹⁸

Gradient flows

Definition

A gradient system is a triple $(\mathcal{Z}, \mathcal{F}, \mathcal{D})$ where $\mathcal{Z}$ is a manifold with a differentiable structure, $\mathcal{F} : \mathcal{Z} \rightarrow \mathbb{R}$ a functional driving the dynamics of the system and $\mathcal{D}(z, \cdot) : T_z \mathcal{Z} \rightarrow \mathbb{R}$ a non-negative convex dissipation potential such that $\mathcal{D}(z, 0) = 0$.

Definition

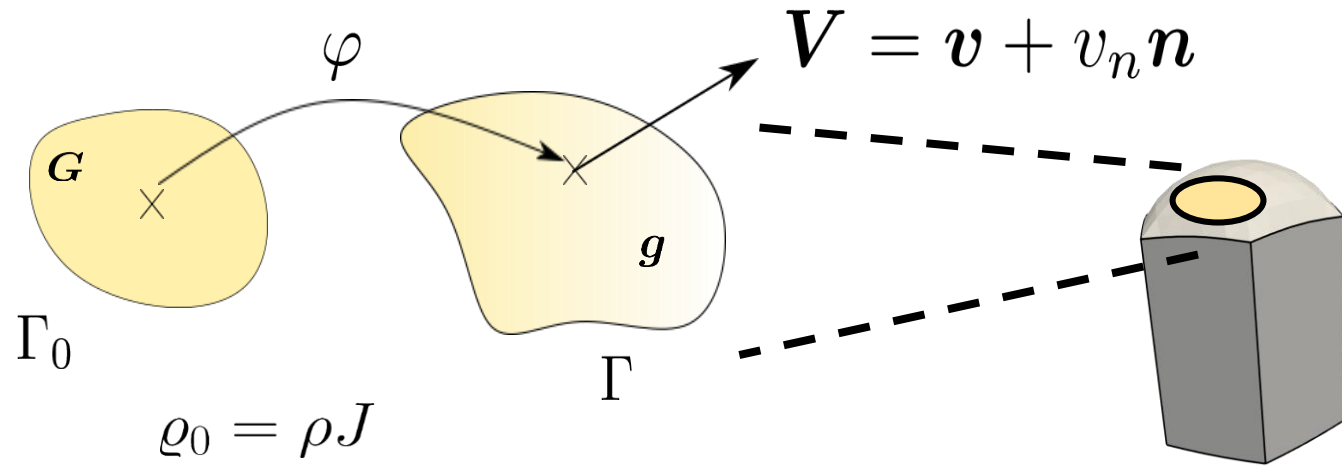
A solution is a curve $z : I \subset \mathbb{R} \rightarrow \mathcal{Z}$ solving the following gradient flow equation

$$\mathcal{G}(z)\dot{z} = -D\mathcal{F}(z) \text{ in } T_z^* \mathcal{Z}$$

- $\mathcal{Z} \rightarrow$ state space
- $\mathcal{F} \rightarrow$ (free) energy
- $\mathcal{D}(z, \dot{z}) = \frac{1}{2} \langle \mathcal{G}(z)\dot{z}, \dot{z} \rangle$ where $\mathcal{G}(z) : T_z \mathcal{Z} \rightarrow T_z^* \mathcal{Z}$ is symmetric positive definite

$$\longrightarrow \frac{d}{dt} \mathcal{F}(z) = \langle D\mathcal{F}(z), \dot{z} \rangle = -\langle \mathcal{G}(z)\dot{z}, \dot{z} \rangle = -2\mathcal{D}(z, \dot{z}) \leq 0$$

Active-viscoelastic-gel description of the cortex

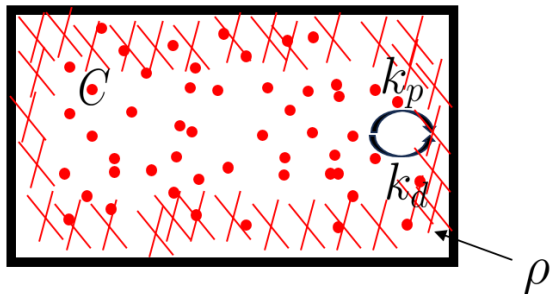


$$\varrho_0 = \rho J$$

$$\mathbf{C} = \varphi^*(\mathbf{g}) \quad \mathbf{d} = \frac{1}{2}(\nabla \mathbf{v} + \nabla \mathbf{v}^T) - v_n \mathbf{k}$$

$$\mathbf{E} = \frac{1}{2}(\mathbf{C} - \mathbf{G}) \longrightarrow (\mathbf{C}, \mathbf{G})$$

$$\frac{d\rho}{dt} + \rho(\nabla \cdot \mathbf{v} + v_n H) = k_p C + k_d \rho \quad \text{turnover}$$



$$\mathcal{F} = \int_{\Gamma_0} \varrho_0 W(\mathbf{C}, \mathbf{G}) dS \quad \text{elasticity}$$

$$\mathcal{D} = \frac{\eta}{2} \int_{\Gamma_0} \varrho_0 \dot{\mathbf{G}} : \dot{\mathbf{G}} dS \quad \text{remodelling}$$

$$\mathcal{P} = \int_{\Gamma} \boldsymbol{\gamma} : \mathbf{d} dS \quad \text{contractility}$$

$\boldsymbol{\gamma}(\rho) = \rho \xi \mathbf{I}$

$$\mathcal{P}_e = - \int_{\partial \Gamma_N} \mathbf{t} \cdot \mathbf{v} dl - \int_{\Gamma} P v_n dS \quad \text{external loads}$$

$$\mathcal{R} = \frac{d\mathcal{F}}{dt} + \mathcal{D} + \mathcal{P} + \mathcal{P}_e$$

Governing equations

Minimization of $\mathcal{R}(X; V) = D_X \mathcal{F}(X) \cdot P(X)V + \mathcal{D}(X; V) + \mathcal{P}(X; V)$

Momentum balance in tangential direction

$$\partial_v \mathcal{R} = 0 \longrightarrow \begin{cases} \nabla \cdot \boldsymbol{\sigma} = 0 \text{ on } \Gamma \\ \boldsymbol{t} = \boldsymbol{\sigma} \boldsymbol{n} \text{ on } \partial\Gamma_N \end{cases}$$

$$\boldsymbol{\sigma} = \boldsymbol{\gamma} + \boldsymbol{\sigma}_e \quad \text{active + elastic tension}$$

Momentum balance in normal direction

$$\partial_{v_n} \mathcal{R} = 0 \longrightarrow \boldsymbol{\sigma} : \boldsymbol{k} = P \text{ on } \Gamma$$

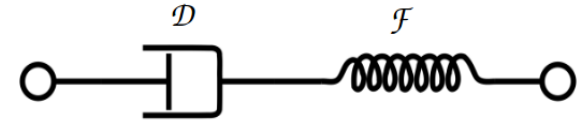
Evolution rule for rate of change of metric

$$\partial_{\dot{G}^{\alpha\beta}} \mathcal{R} = 0 \longrightarrow \dot{G}^{\alpha\beta} = -\frac{1}{2\rho_0\eta} G^{\alpha\gamma} C_{\gamma\delta} S_e^{\delta\beta}$$

Assuming Neo-hookean material

Multidimensional extension of Maxwell model :

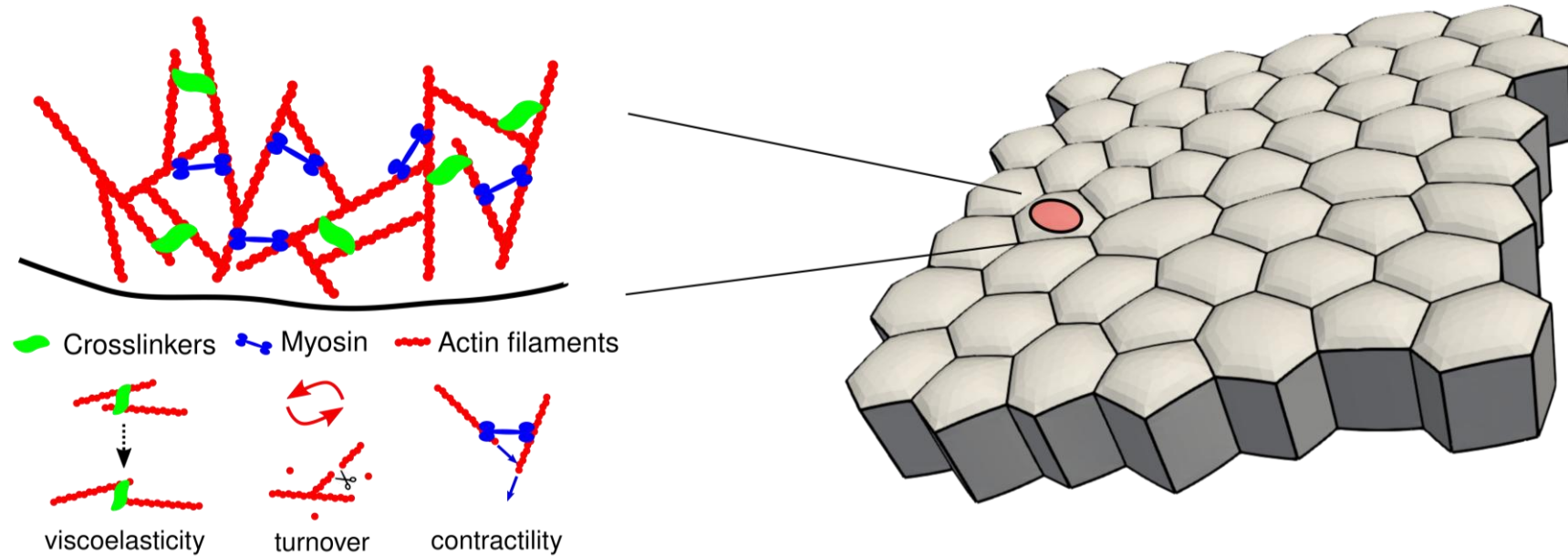
- Very short timescale : active hyperelastic behaviour
- Longer timescales : active viscoelastic behaviour



$$\tau_r = \frac{\eta}{\mu}$$

$$\tau_t = \frac{1}{k_d}$$

Tissues as a collection of active gels



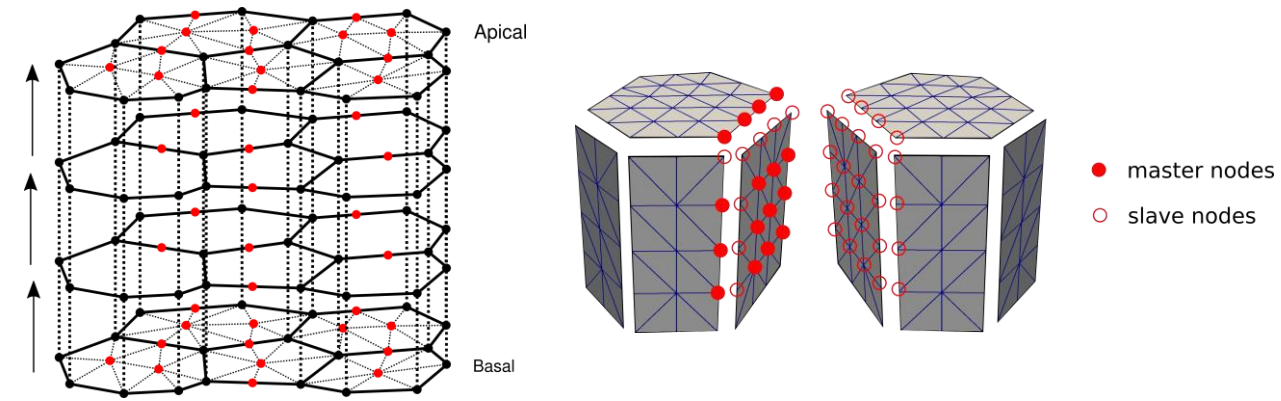
Cell level

$$\mathcal{L}_c(X_c; V_c, P_c) = \mathcal{R}_c(X_c; V_c) - P_c \dot{\Omega}_c$$

Tissue level

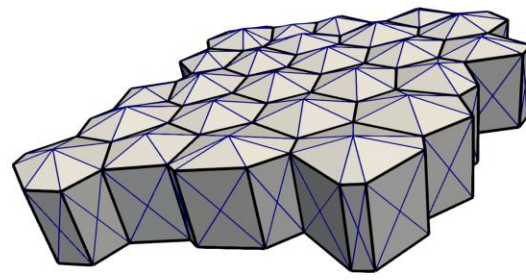
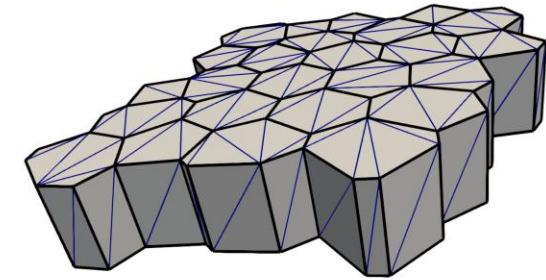
$$\mathcal{L}_m(X_m; V_m, \lambda_m) = \sum_{c \in \langle t \rangle} \mathcal{L}_c(X_c; V_c, P_c)$$

Mesh generation and finite element discretization



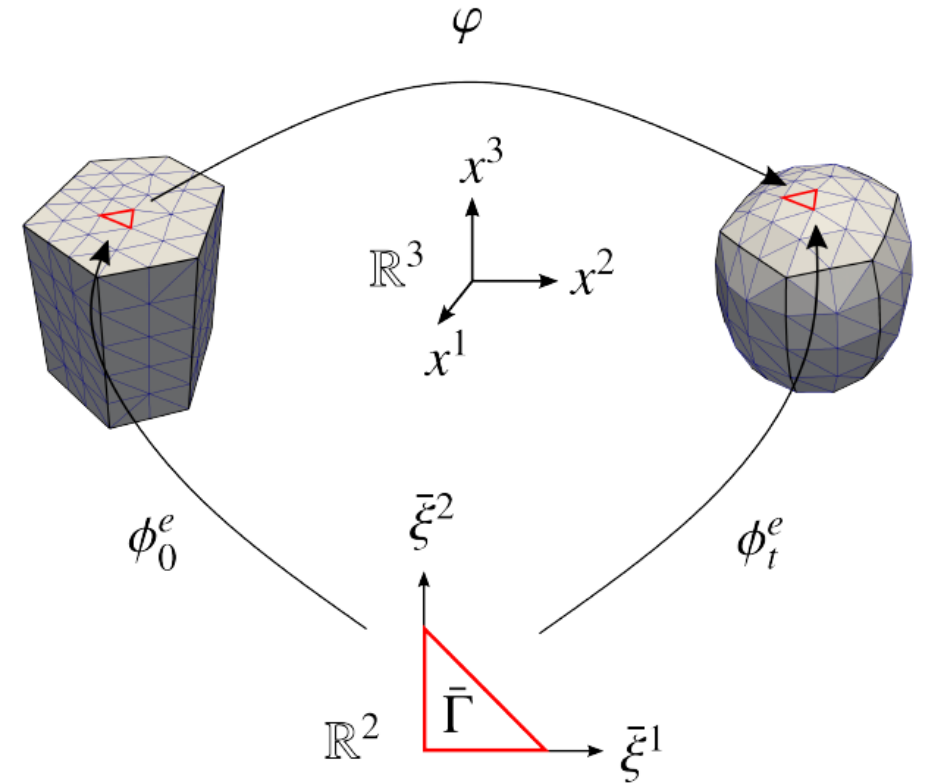
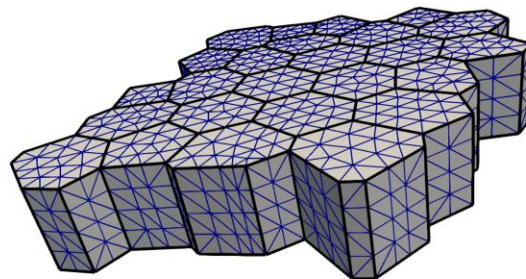
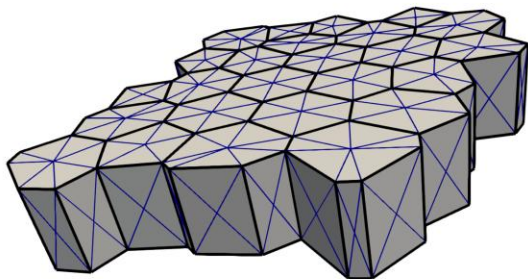
a

b



c

d



implicit backward-Euler variational integrator

$$\mathbf{V}_I^{n+1} \approx \frac{\mathbf{x}_I^{n+1} - \mathbf{x}_I^n}{\Delta t^n} \quad \dot{\mathbf{G}}_{f,c}^{n+1} \approx \frac{\mathbf{G}_{f,c}^{n+1} - \mathbf{G}_{f,c}^n}{\Delta t^n}$$

$$\dot{\mathcal{F}}_{f,c} [\phi, \rho_{f,c}, \mathbf{G}_{f,c}; \mathbf{V}, \dot{\mathbf{G}}_{f,c}] \approx \frac{1}{\Delta t^n} \mathcal{F}_{f,c} [\{\mathbf{x}_I^{n+1}, \mathbf{G}_{f,c}^{n+1}\}]$$

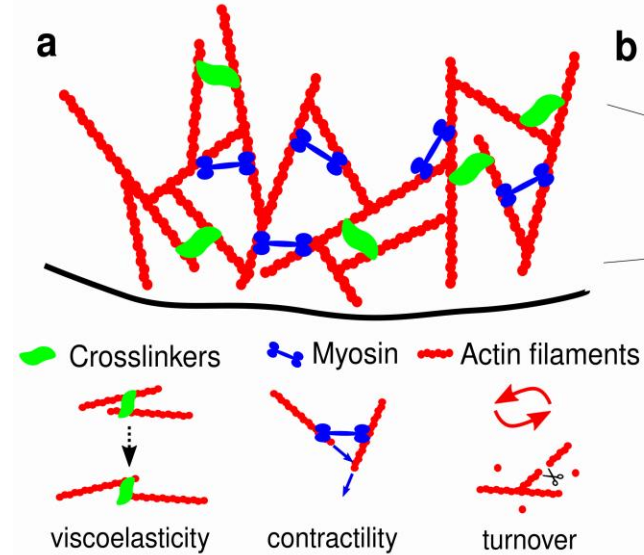
$$\mathcal{D}_{f,c} [\phi, \rho_{f,c}, \mathbf{G}_{f,c}; \dot{\mathbf{G}}_{f,c}] \approx \mathcal{D}_{f,c} \left[\{\mathbf{x}_I^n, \mathbf{G}_{f,c}^n, \rho_{f,c}^n\} ; \left\{ \frac{\mathbf{G}_{f,c}^{n+1} - \mathbf{G}_{f,c}^n}{\Delta t^n} \right\} \right]$$

$$\mathcal{P}_{f,c} [\phi, \rho_{f,c}; \mathbf{V}] \approx \mathcal{P}_{f,c} \left[\{\mathbf{x}_I^n, \rho_{f,c}^n\} ; \left\{ \frac{\mathbf{x}_I^{n+1} - \mathbf{x}_I^n}{\Delta t^n} \right\} \right]$$

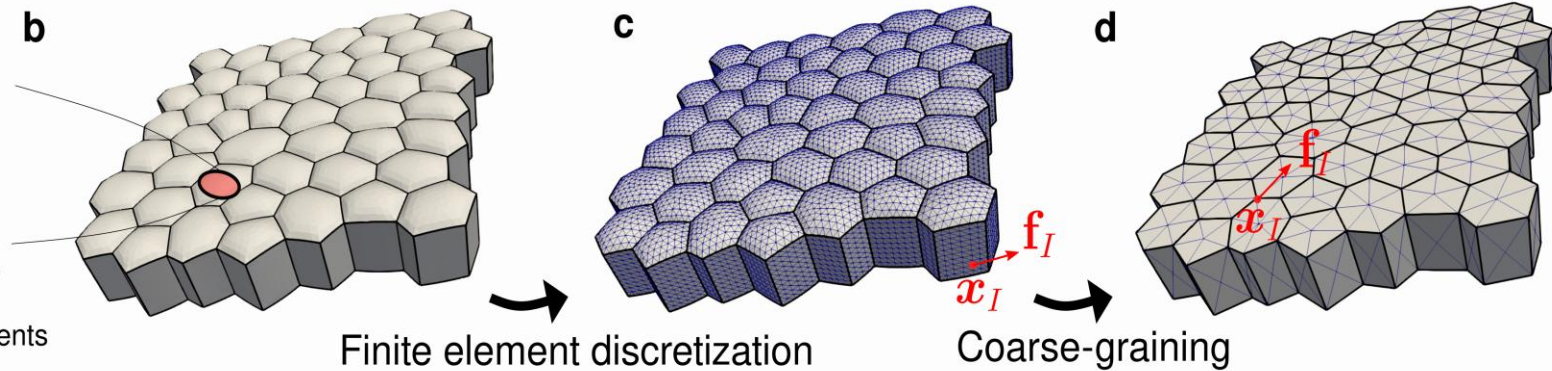
$$P_c \dot{\Omega}_c \approx P_c^{n+1} \frac{\Omega_c (\{\mathbf{x}_I^{n+1}\}) - \Omega_c (\{\mathbf{x}_I^n\})}{\Delta t^n}$$

Discrete governing equations

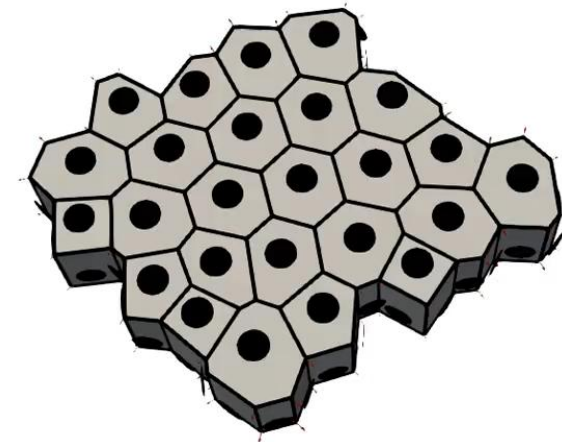
Active-viscoelastic gel



Dynamic vertex model



Cortical Thickness
 1.20
 0.800

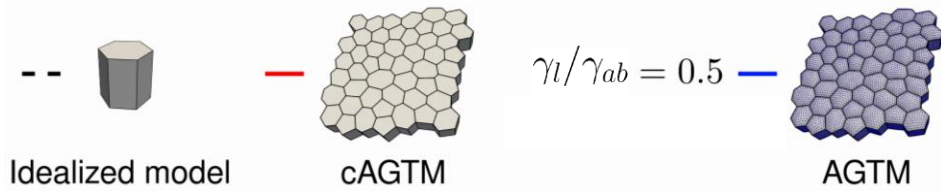
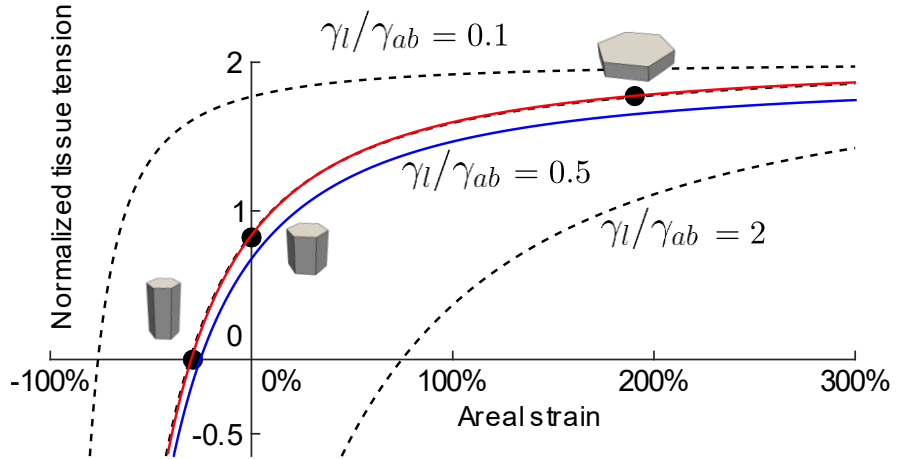
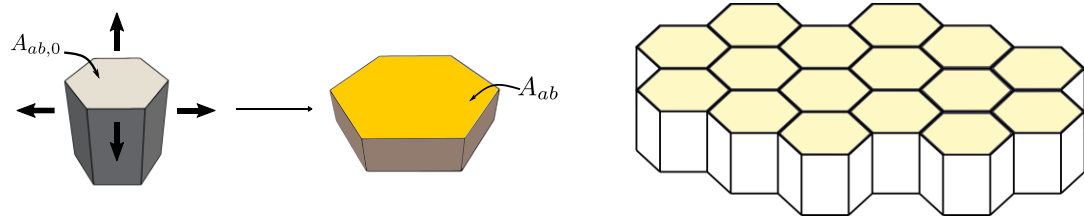


$$\begin{cases} \rho_{f,c}^{n+1} - \rho_{f,c}^n - \Delta t^n \left[k_p C_0 - \rho_{f,c}^{n+1} \left(\frac{j_{f,c}^{n+1}}{J_{f,c}^n} + k_d \right) \right] = 0 \\ \{\mathbf{x}_I^{n+1}, \mathbf{G}_{f,c}^{n+1}, P_c^{n+1}\} = \arg \min_{\{\mathbf{x}_I, \mathbf{G}_{f,c}\}} \arg \max_{P_c} (\mathcal{L}_m [\{\mathbf{x}_I^n, \rho_{f,c}^n, \mathbf{G}_{f,c}^n\}; \{\mathbf{x}_I, \mathbf{G}_{f,c}\}, \{P_c\}]) \end{cases}$$

**Solving an active gel on each
curved face of each cell**

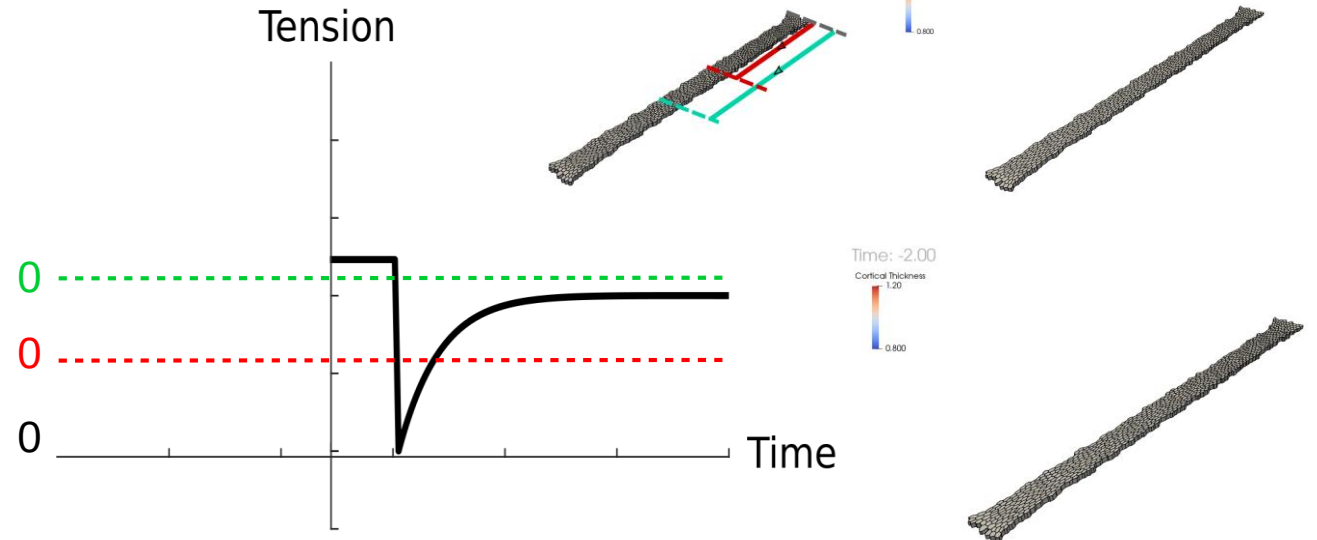
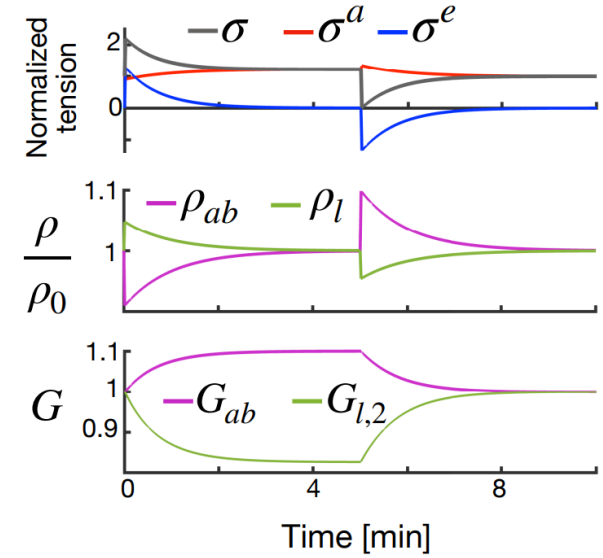
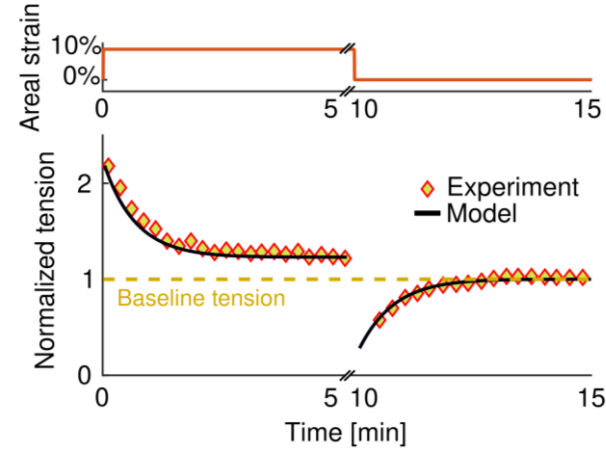


Tissue response under stretch

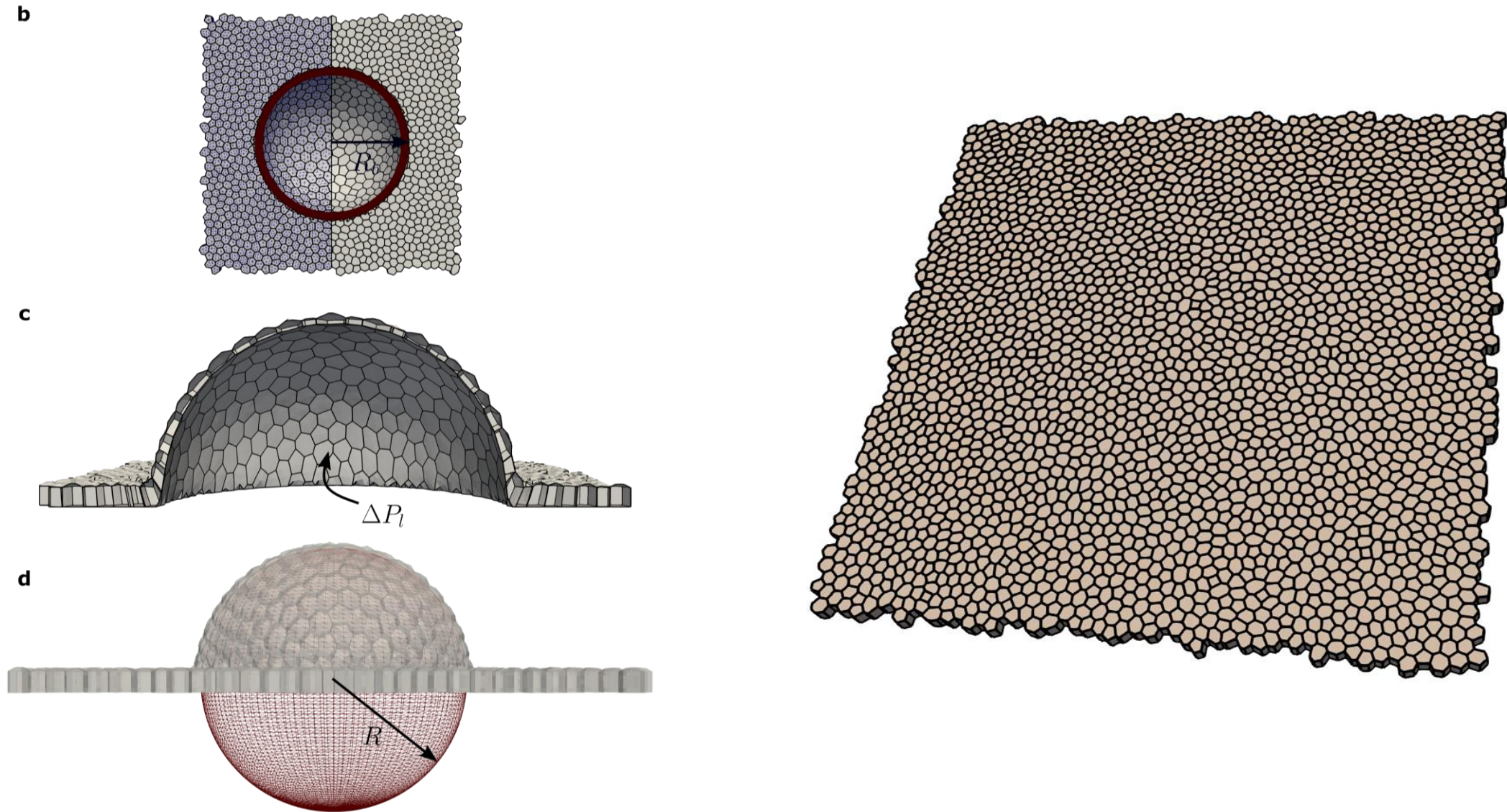


$$\sigma = 2 - \frac{\xi_l}{\xi_{ab}(\varepsilon_{ab} + 1)^{3/2}} \frac{k}{\xi_{ab}(\varepsilon_{ab} + 1)^{3/2}}$$

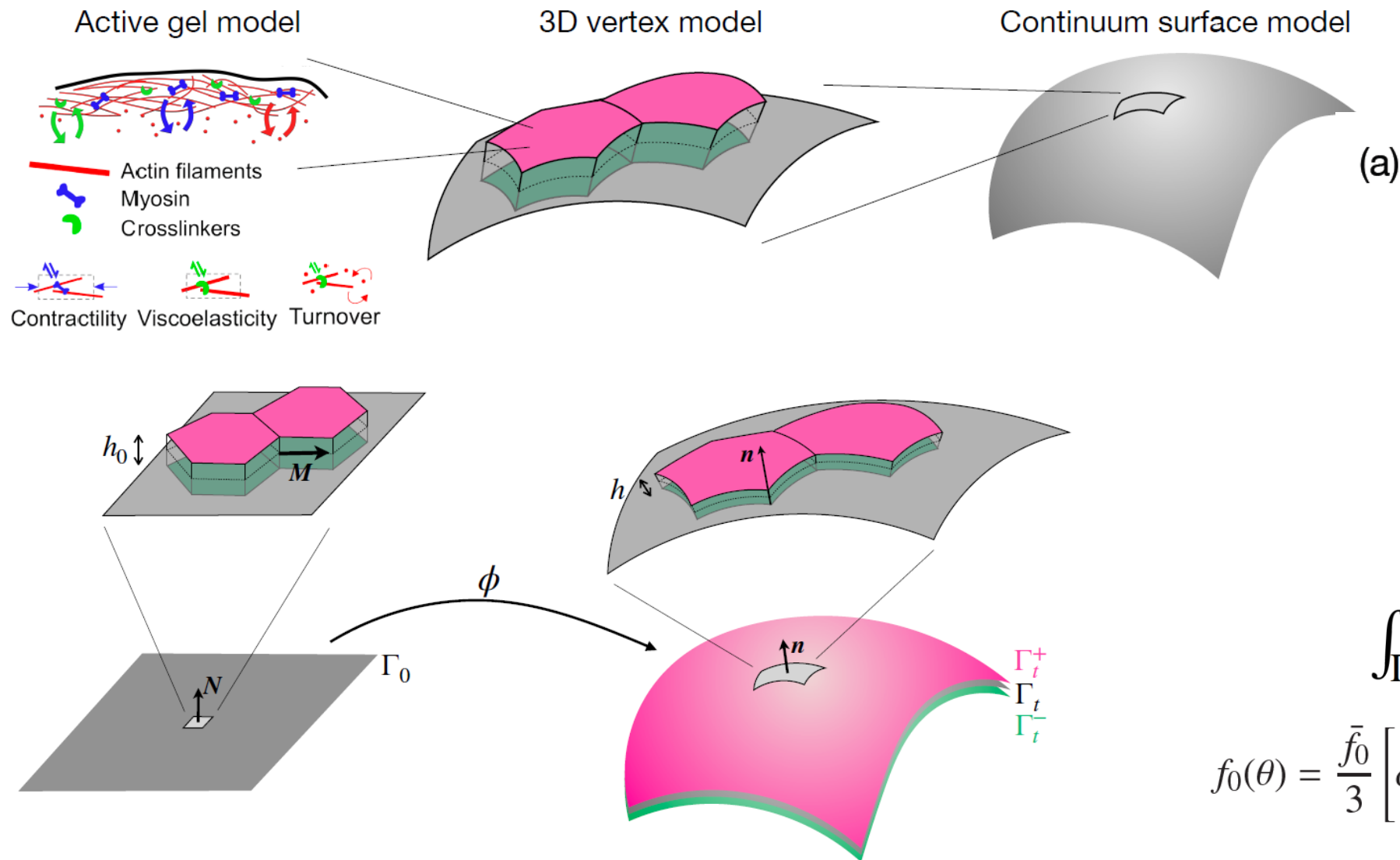
$$\varepsilon_{ab} = \frac{A_{ab}}{A_{ab,0}} - 1$$



Mechanics of epithelial domes : CVM



Continuum Kirchhoff theory for epithelial shells



$$\int_{\Gamma_0} \int_0^\pi f_0(\mathbf{X}, \theta) d\theta dS_0$$

$$f_0(\theta) = \frac{\bar{f}_0}{3} \left[\delta(\theta) + \delta\left(\theta - \frac{\pi}{3}\right) + \delta\left(\theta - \frac{2\pi}{3}\right) \right]$$

$$\bar{f}_0 = \frac{2\sqrt{3}h_0}{3\ell_0}$$

Continuum Kirchhoff theory for epithelial shells

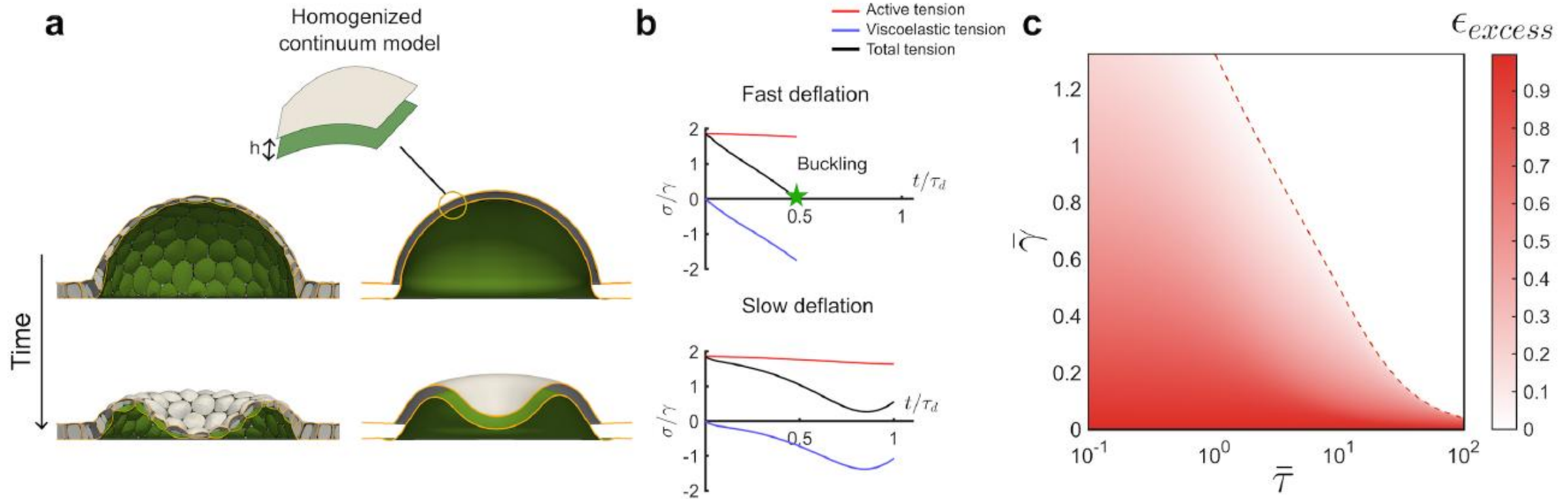


$$\begin{aligned} \mathcal{R}[\dot{\varphi}, \dot{\mathbb{G}}^{\pm}, \dot{\mathbb{G}}^L] = & \int_{\Gamma_0} \left[\frac{1}{2} \mathbf{S}^{\text{eff}} : \dot{\mathbf{C}} + \mathbf{m}^{\text{eff}} : \dot{\mathbf{k}} \right] dS_0 + \int_{\Gamma_0} \frac{\tilde{\eta}_m}{2} |\mathbf{V}|^2 J^{\text{mid}} dS_0 \\ & + \int_{\Gamma_0} \left[\sum_{\alpha=\pm} \left(\frac{\partial \Psi^\alpha}{\partial \mathbb{G}^\alpha} : \dot{\mathbb{G}}^\alpha + \Phi^\alpha(\dot{\mathbb{G}}^\alpha) \right) \varrho_0^\alpha \frac{G^\alpha}{G} + \int_0^\pi \left(\frac{\partial \Psi^L}{\partial \mathbb{G}^L} : \dot{\mathbb{G}}^L + \Phi^L(\dot{\mathbb{G}}^L) \right) \varrho_0^L f_0(\theta) d\theta \right] dS_0, \end{aligned}$$

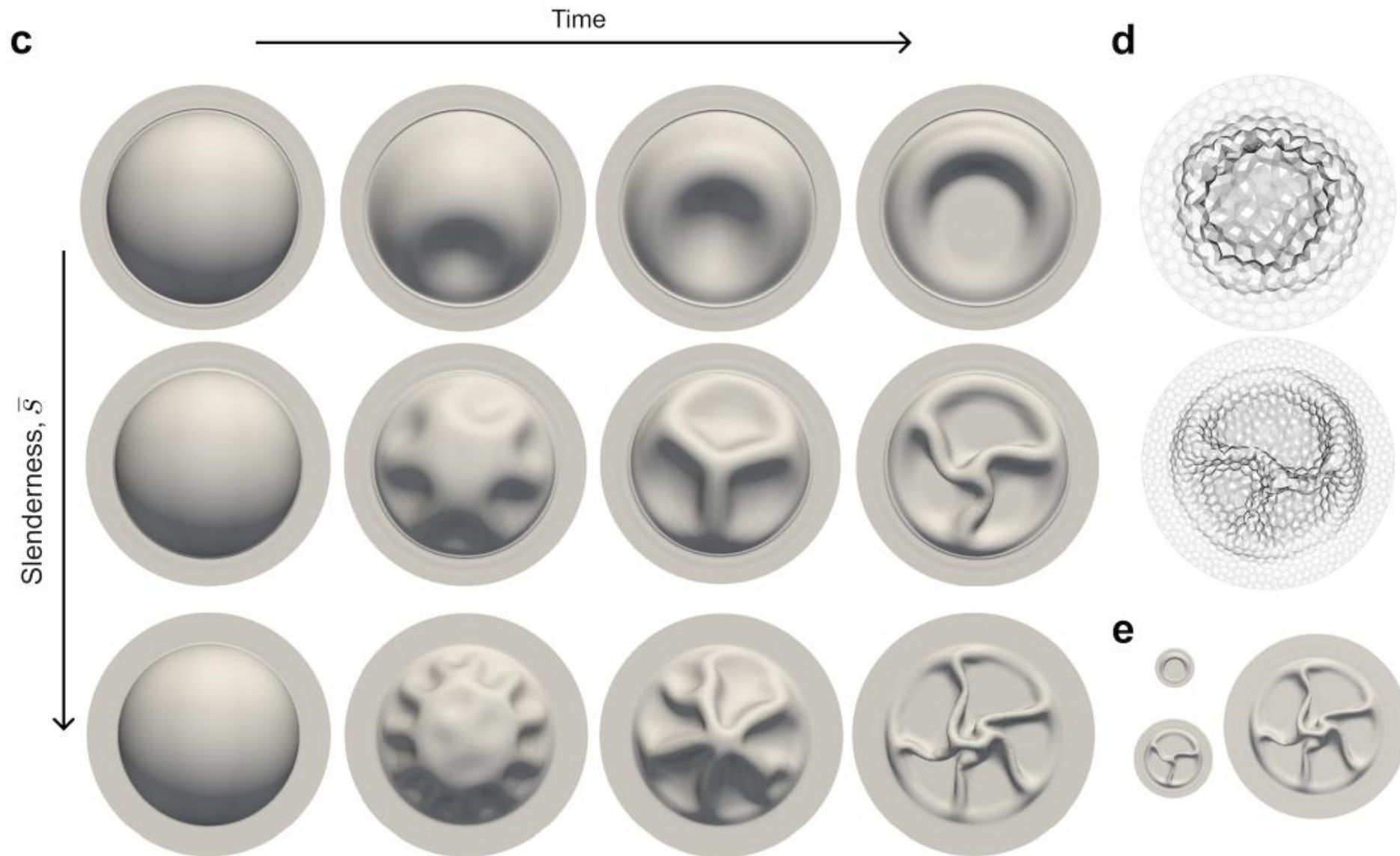
$$\mathbf{S}^{\text{eff}} = \mathbf{S}^+ + \mathbf{S}^- + \frac{h}{4} [(\mathbf{S}^+ + \mathbf{S}^-) : \mathbf{k}] \mathbf{C}^{-1} + \int_0^\pi \left(S_{MM}^L \mathbf{M} \otimes \mathbf{M} - \frac{1}{J^{\text{mid}^2}} S_{NN}^L \mathbf{C}^{-1} \right) f_0(\theta) d\theta$$

$$\mathbf{m}^{\text{eff}} = -\frac{h}{4} (\mathbf{S}^+ - \mathbf{S}^-)$$

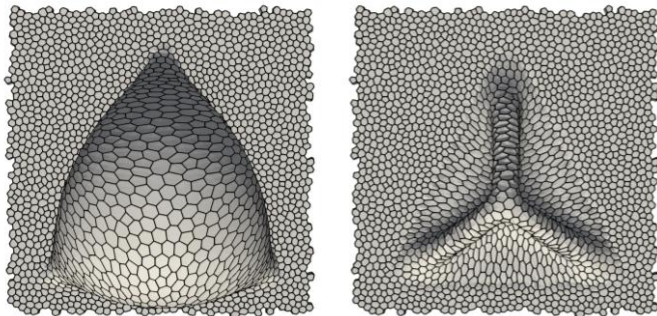
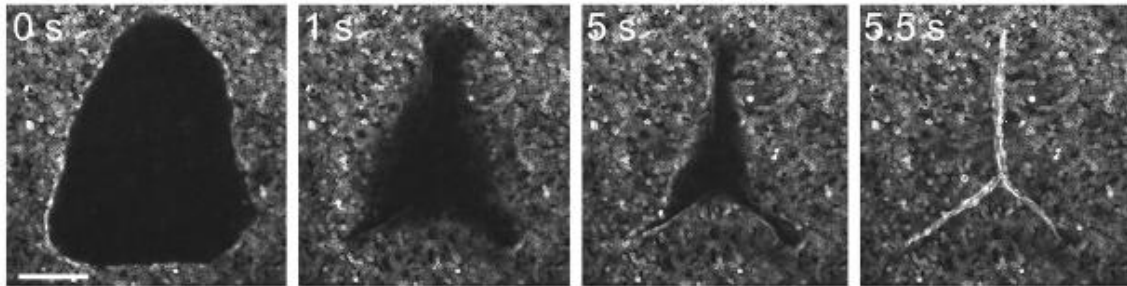
Buckling phase diagram



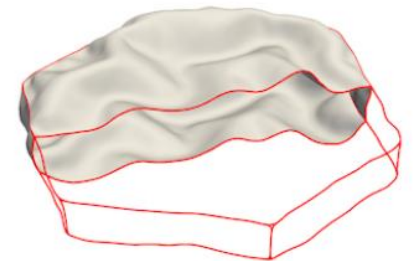
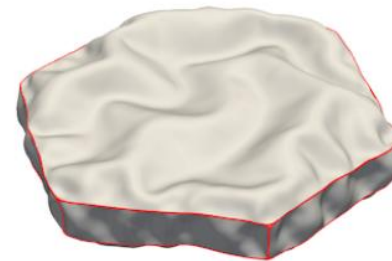
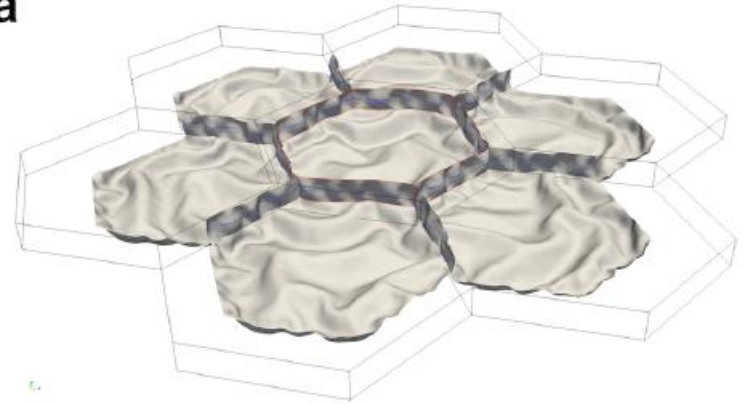
Symmetry breaking and wrinkle-to-fold transition



Engineering folds



a



Conclusion and further work

- Established mechanical rules for unsupported epithelial buckling (intrinsic mechanical properties)
- Explored new regime of buckling dynamics across a broad range of time scales, length scales, geometries, and mechanical properties of the epithelium
- Rational design of folds
- Epithelial buckling as a stress-buffering and morphogenetic mechanism
- Analytical arguments for active wrinkles and folds
- “Geometrical morphogens”

Collaborators



Marino Arroyo



Sohan Kale



Alejandro
Torres-
Sánchez



Daniel
Santos-
Oliván



Pradeep K. Bal



Guillermo
Vilanova



Xavier Trepát

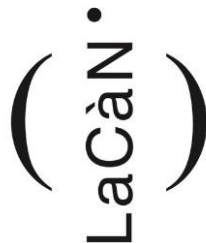


Nimesh
Chahare

Thank you for your
attention



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BARCELONATECH



SORBONNE
UNIVERSITÉ ²⁹

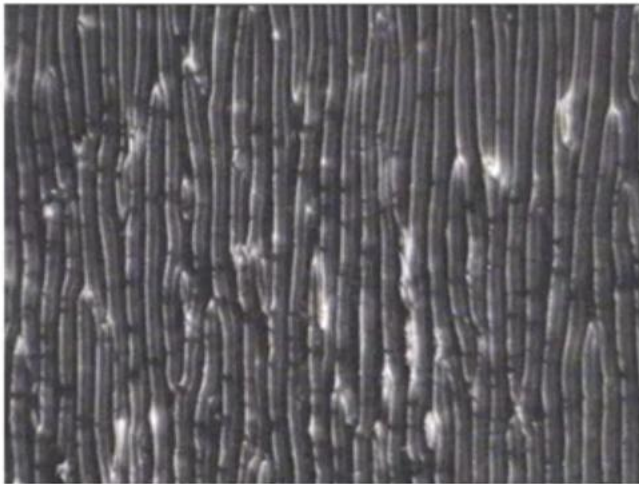
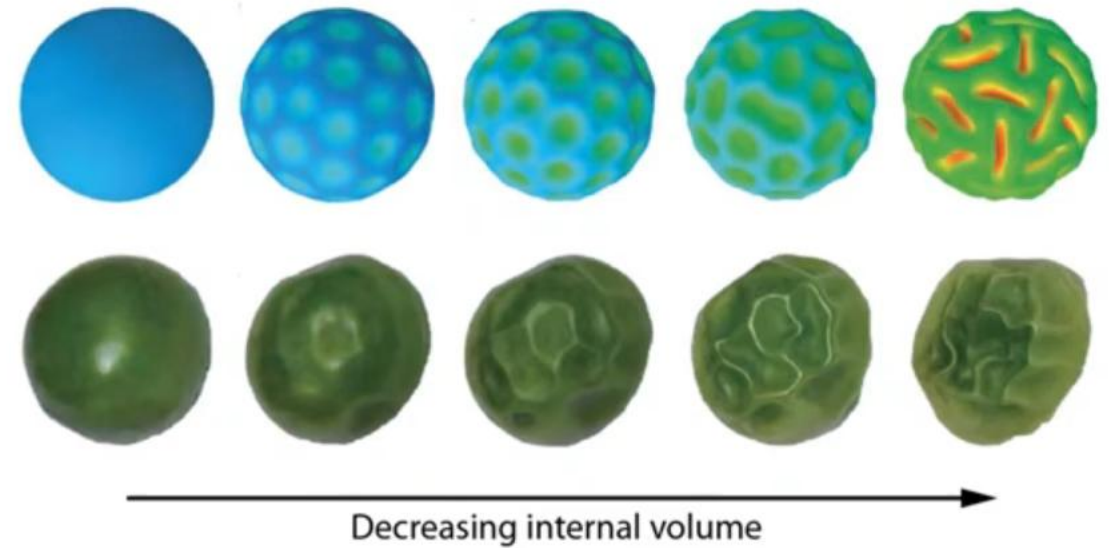


Extra slides

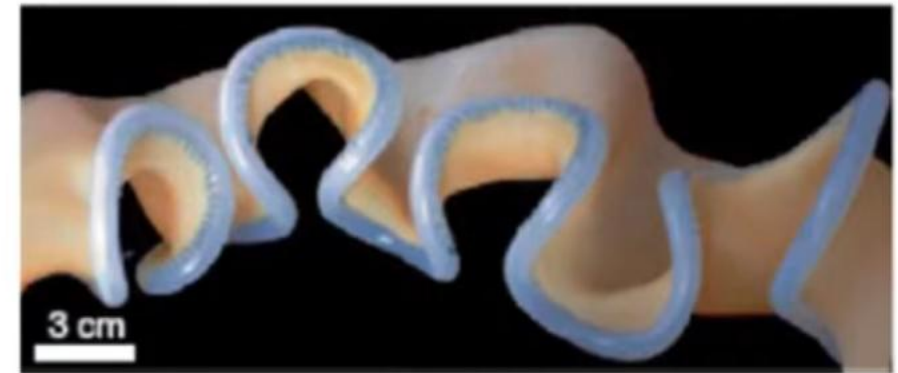
Three types of wrinkles

- Three ways wrinkles arise
 - Constrained volume change
 - Hard and soft layers
 - Mismatched deformation systems

Images below: Li, Bo, Yan-Ping Cao, Xi-Qiao Feng, and Huajian Gao. *Soft Matter* 8, no. 21 (2012): 5728-5745



Multilayer system with hard surface layer and soft interior



Orange rubber was stretched then attached to blue rubber